

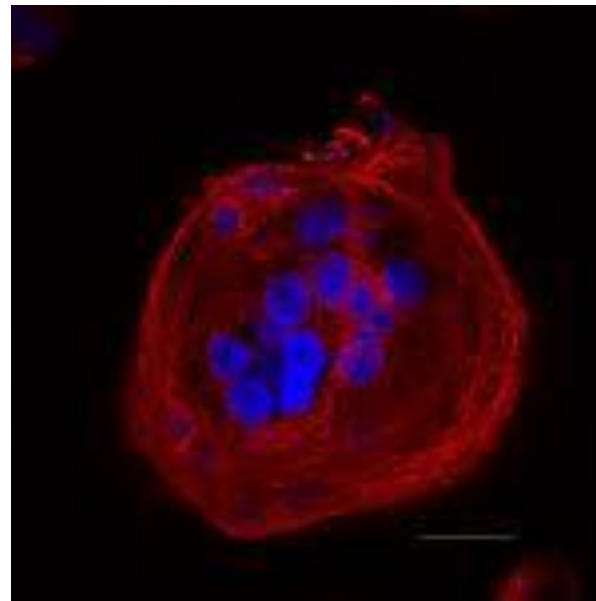
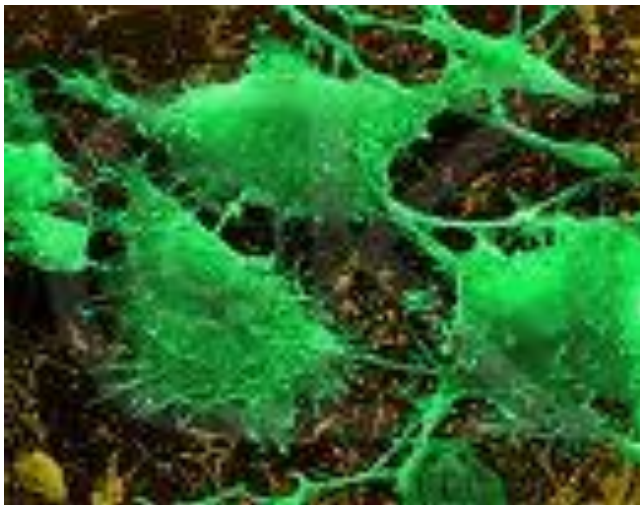


# ***Quantitative Fluorescence Microscopy for the Study of Protein Interactions, Signaling, and Molecular Microenvironment***

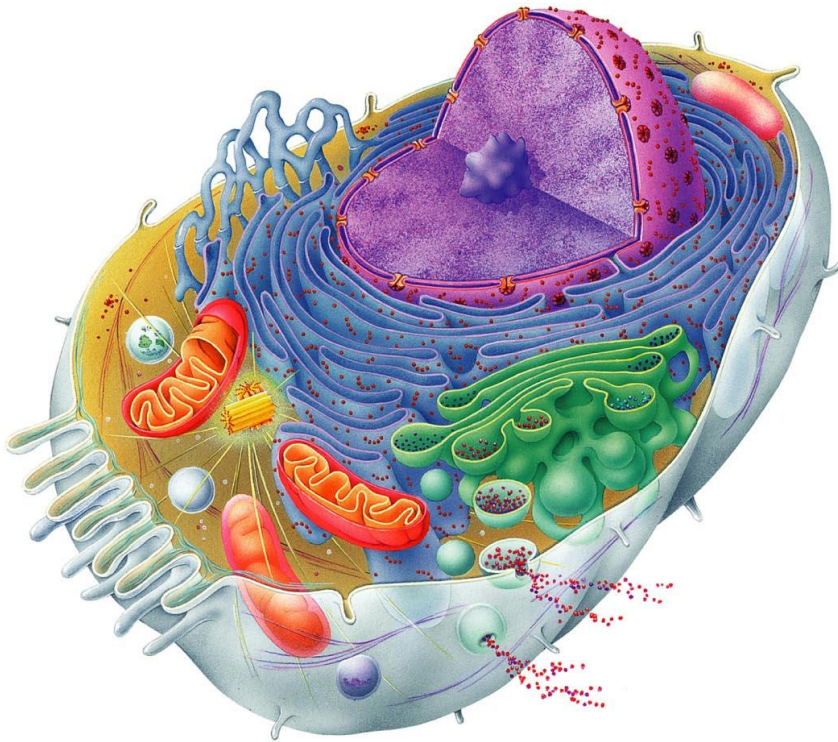
Advanced Fluorescence Microscopy Workshop, Urbana-Champaign Aug. 17-20 2015

**Beniamino Barbieri**

# Cell Images



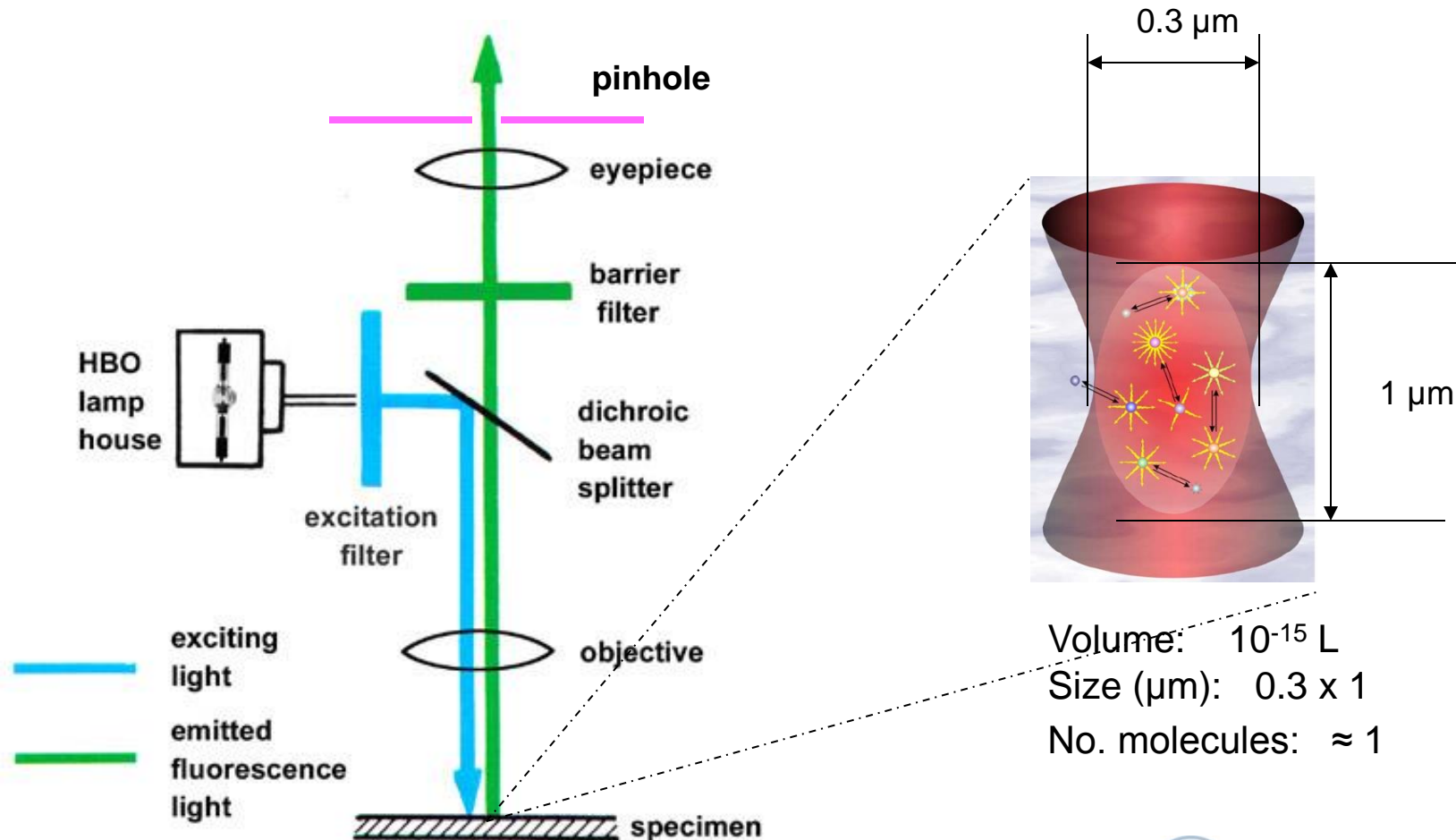
# Cell Structure



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- In a cell we may want to locate the areas where we have clusters of molecules versus single molecules.
- In cells, both the concentration and the clustering of proteins can differ in various locations and change during biological processes.

# Fluorescence microscope



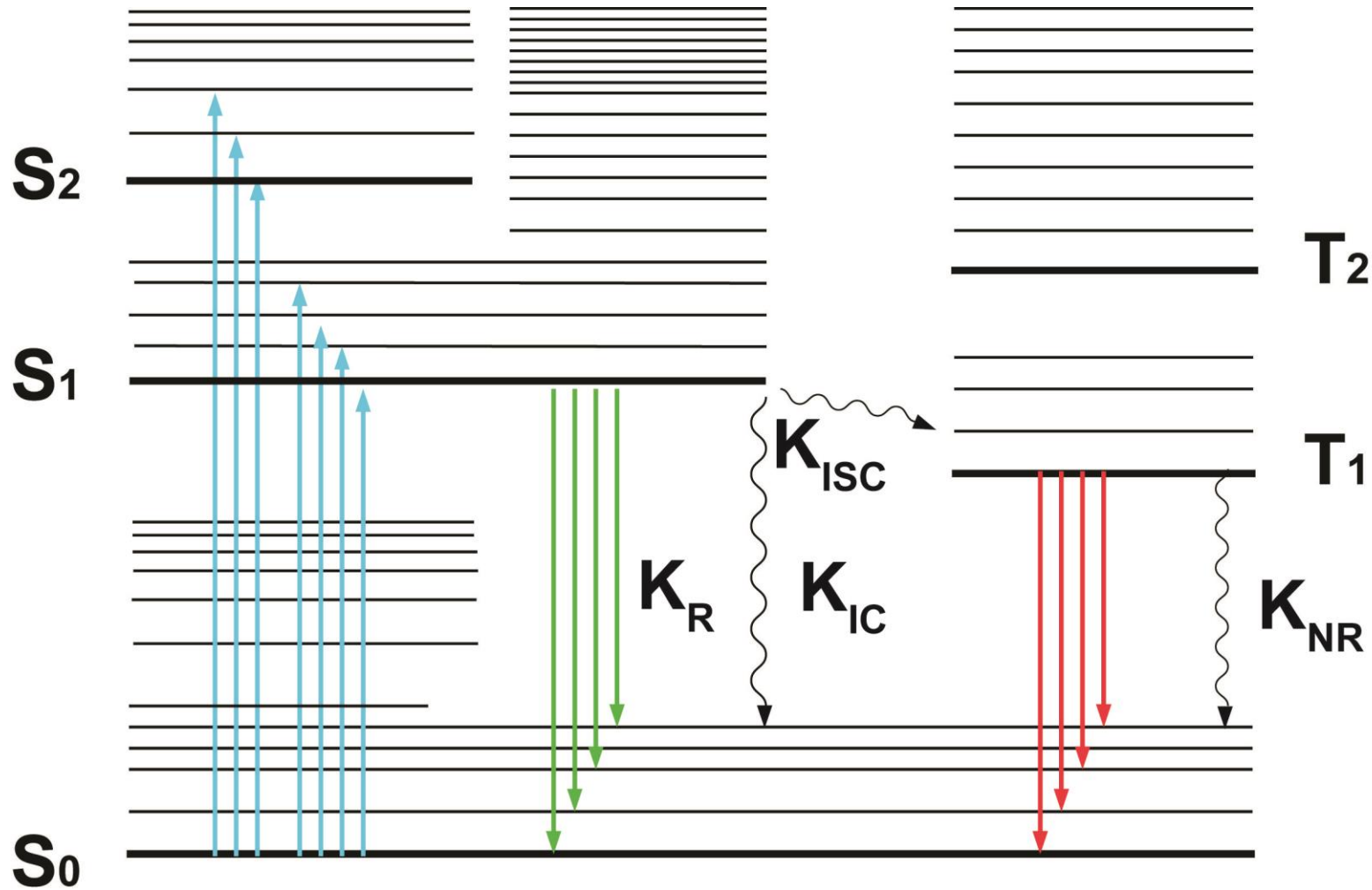
# What is Fluorescence?

**FLUORESCENCE** is the light emitted by an atom or molecule after a finite duration subsequent to the absorption of photons.

Specifically, the emitted light arises from the transition of the excited species from its first excited electronic singlet level to its ground electronic level.

The development of highly sophisticated fluorescent probe chemistries, new lasers and microscopy approaches and site-directed mutagenesis has led to many novel applications of fluorescence in the chemical, physical and life sciences. Fluorescence methodologies are now widely used in the biochemical and biophysical areas, in clinical chemistry and diagnostics and in cell biology and molecular biology.

# Perrin-Jabłoński diagram



# Fluorescence Tools

- Fluorescence Fluctuation Spectroscopy (FFS)
- Fluorescence Lifetime Imaging (FLIM)
- Particle Tracking and nanoimaging

# What is Fluorescence Fluctuations Spectroscopy (FFS)

## Single point

- FCS (Magde, Elson and Webb, 1972)
- PCH (Chen et al., 1999)
- FIDA (Kask et al., 1999)
- FCA (Mueller, 2004)

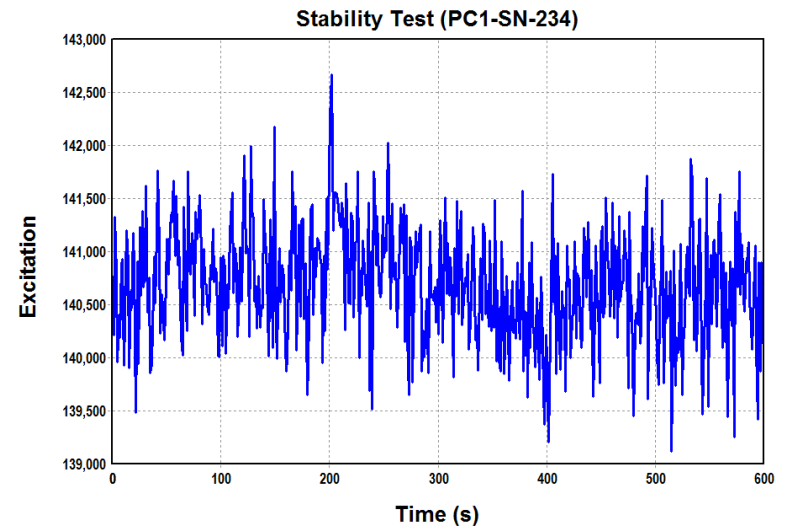
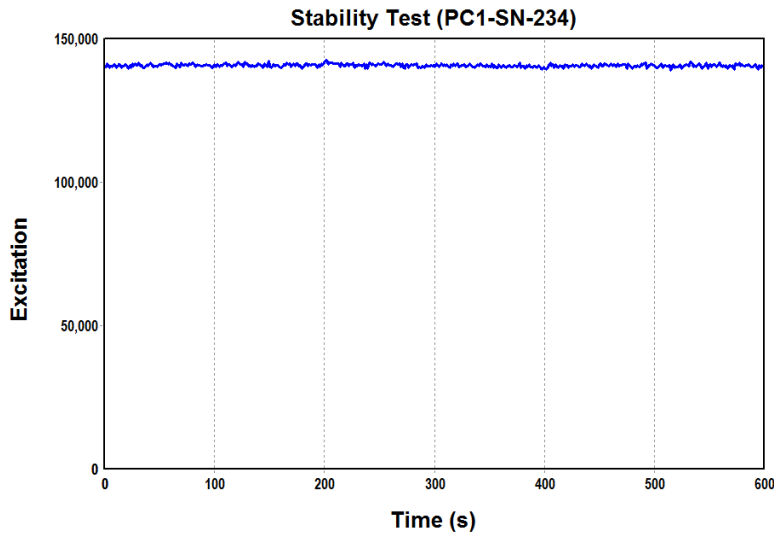
## Imaging

- ICS (Peterson et al. 1993)
- RICS (Digman et al. 2005)
- N & B (Digman et al., 2008)

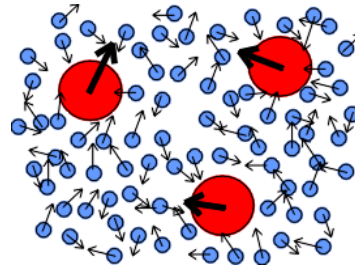


# Fluorescence: is it noise?

## Acquisition of a steady fluorescence signal over time



**Brownian motion**



# Why do we need FFS to measure the internal dynamics in cells?

## Methods based on perturbation

Typically FRAP (fluorescence recovery after photobleaching)

## Methods based on fluctuations

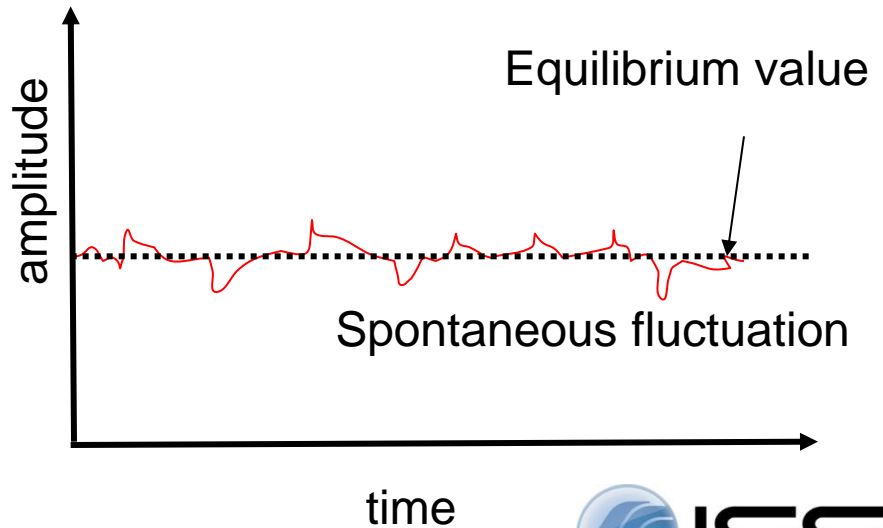
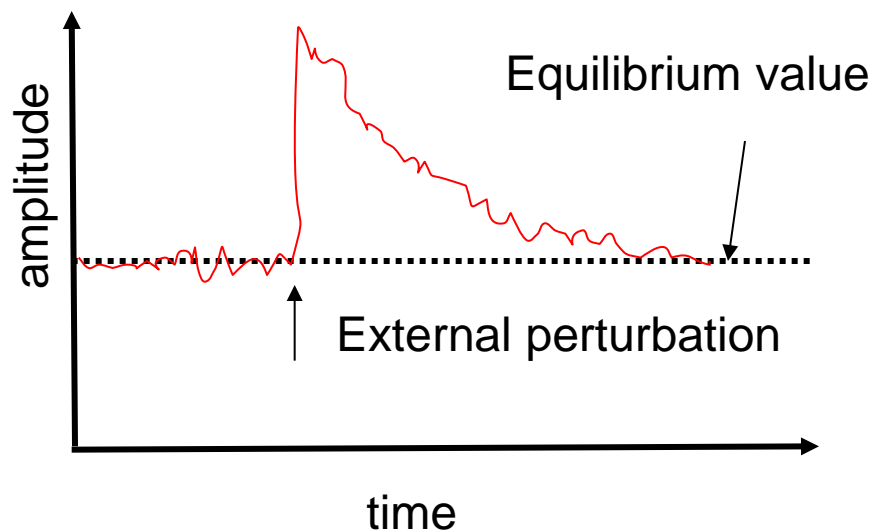
Typically FCS and dynamic ICS methods

There is a fundamental difference between the two approaches, although they are related as to the physical phenomena they report on.

# The fluctuation-dissipation principle

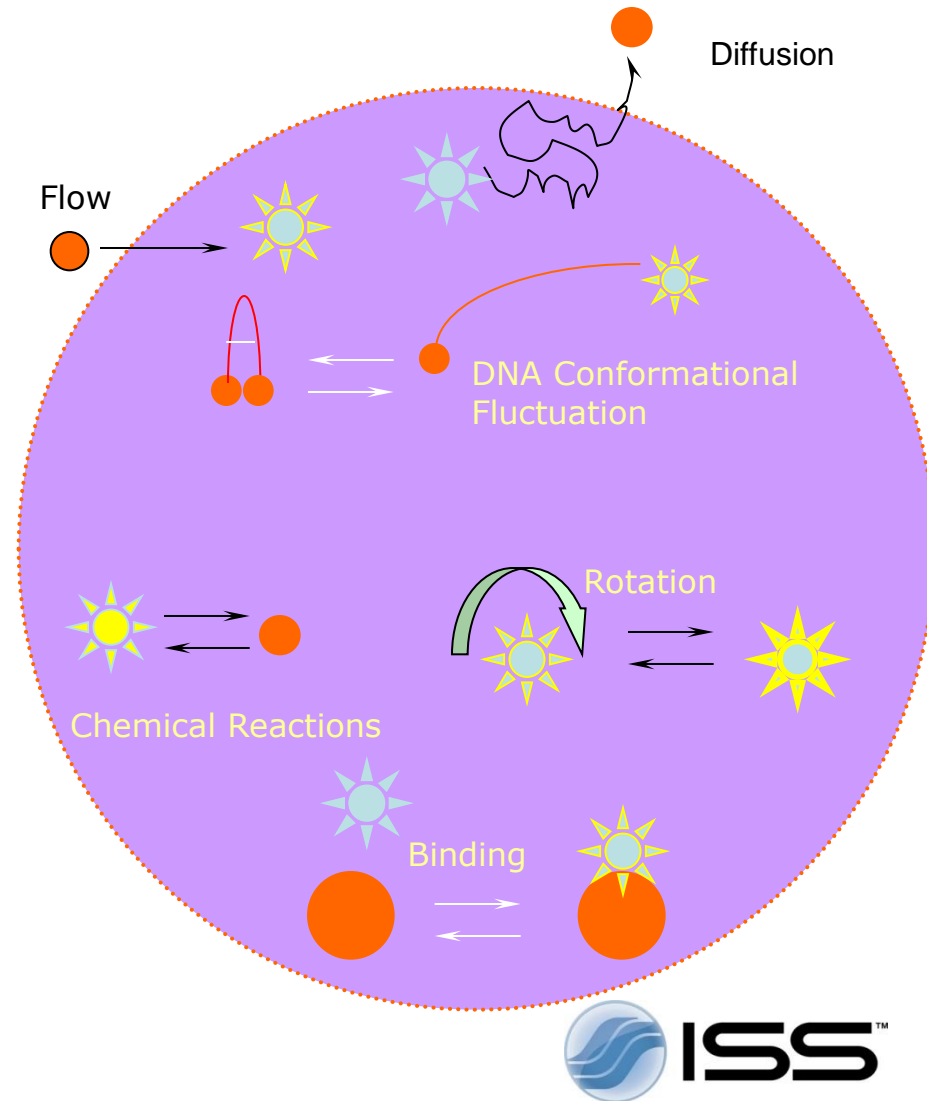
If we perturb a system from **equilibrium**, it returns to the average value with a characteristic time that depends on the process responsible for returning the system to equilibrium

**Spontaneous** energy fluctuations in a part of the system, can cause the system to locally go out of equilibrium. These spontaneous fluctuations **dissipate** with the same time constant as if we had externally perturbed the equilibrium of the system.



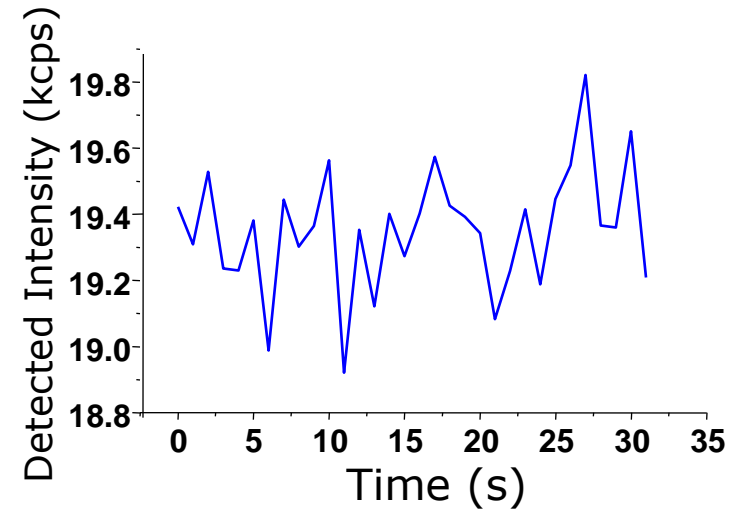
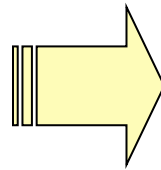
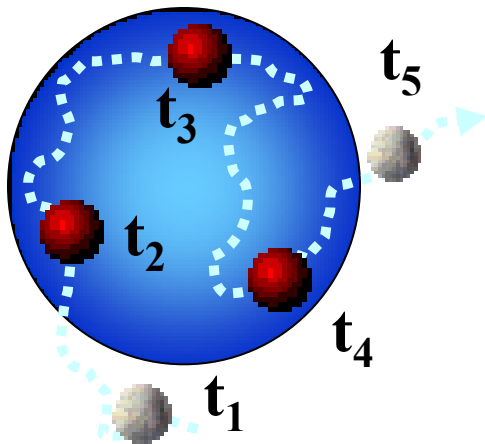
# What can cause a fluctuation in the fluorescence?

- Number of fluorescent molecules in the volume of observation
- Diffusion or binding
- Conformational Dynamics
- Rotational Motion
- Protein Folding
- Blinking
- And many more



# The Signal

## Role of the confocal volume



# How to extract the information about the fluctuations and their characteristic time?

Distribution of the **duration** of the fluctuations

Distribution of the **amplitude** of the fluctuations

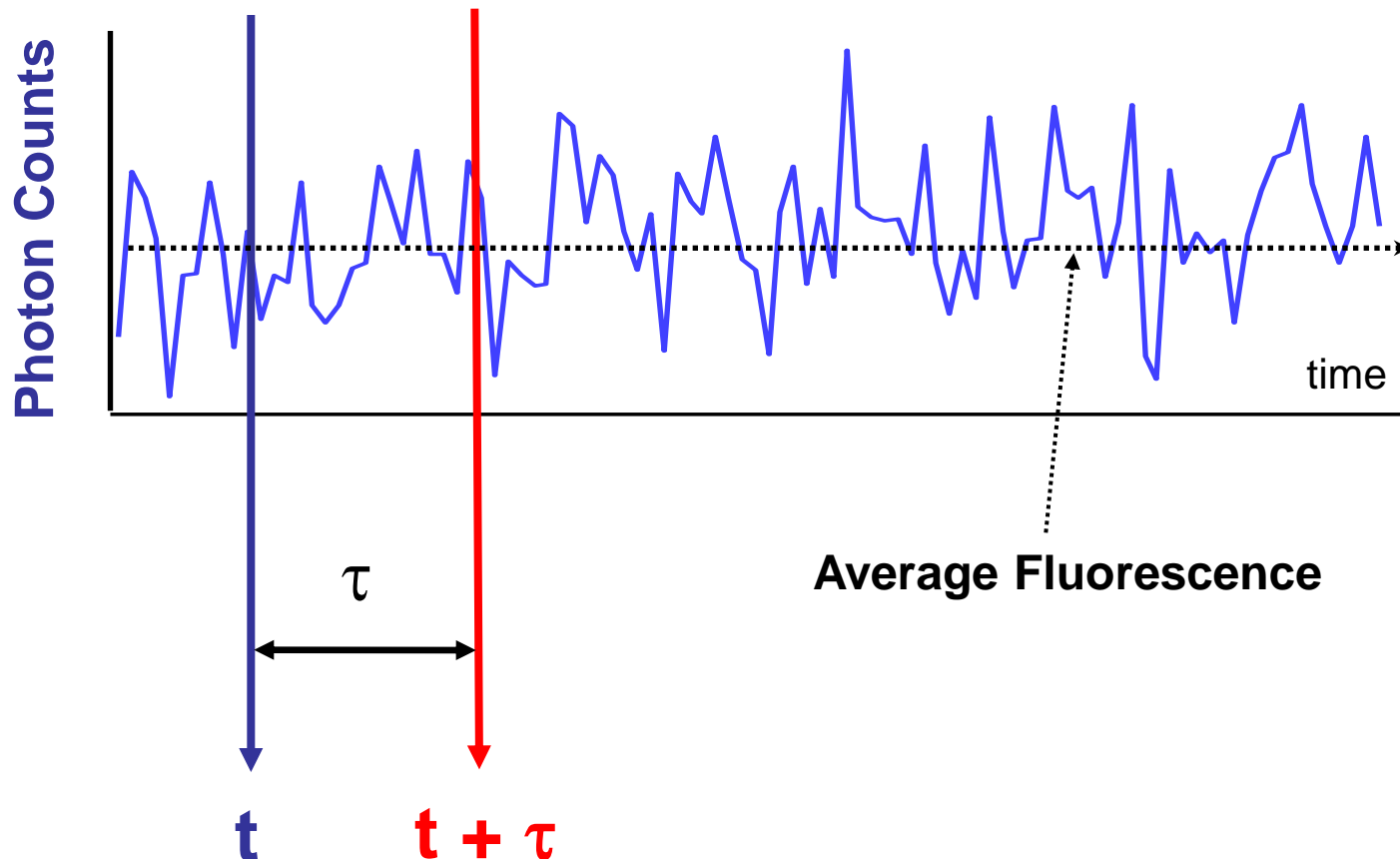
To extract the distribution of the duration of the fluctuations we use a math based on calculation of the **correlation function**

To extract the distribution of the amplitude of the fluctuations, we use a math based on the **PCH distribution**

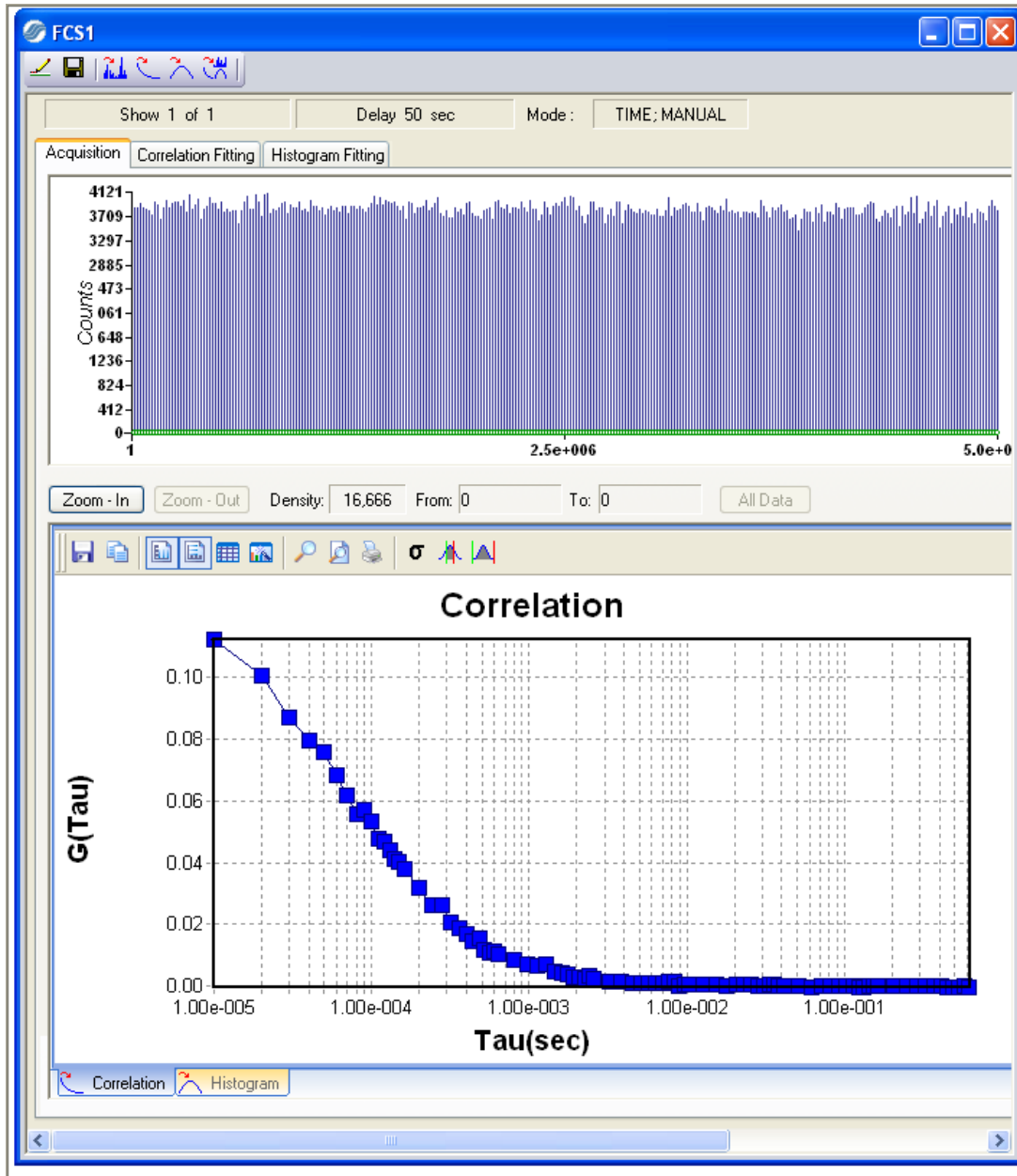
# The definition of the Autocorrelation Function

$$\delta F(t) = F(t) - \langle F(t) \rangle$$

$$G(\tau) = \frac{\langle \delta F(t) \delta F(t + \tau) \rangle}{\langle F(t) \rangle^2}$$



# The autocorrelation function





# What determines the intensity of the fluorescence signal?

**This is the fundamental equation in FCS**

$$F(t) = \kappa Q \int W(\mathbf{r}) C(\mathbf{r}, t) d\Omega$$

$\kappa Q$  = quantum yield and detector sensitivity (how bright is our probe). This term could contain the fluctuation of the fluorescence intensity due to internal processes

$W(\mathbf{r})$  describes the profile of illumination

$C(\mathbf{r}, t)$  is a function of the fluorophore concentration over time. This is the term that contains the “physics” of the diffusion processes

**The value of  $F(t)$  depends on the profile of illumination!**

# The role of the observation volume

$$F(x, y, z) = I_0 I(z) e^{-\frac{2(x^2 + y^2)}{w_0^2}}$$

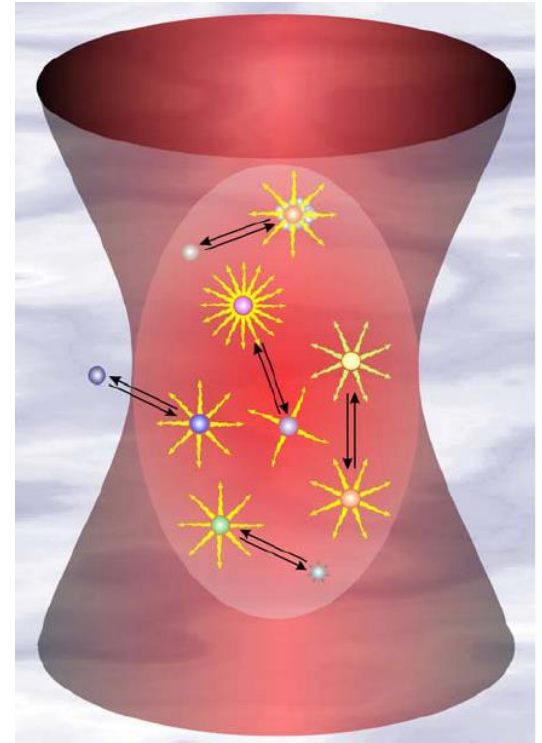
$$I(z) = \text{Exp}\left[-\frac{2z^2}{w_{0z}^2}\right] \quad \text{z-Gaussian}$$

$$I(z) = \frac{1}{1 + \left(\frac{z}{w_{oz}}\right)^2} \quad \text{z-Lorentzian}$$

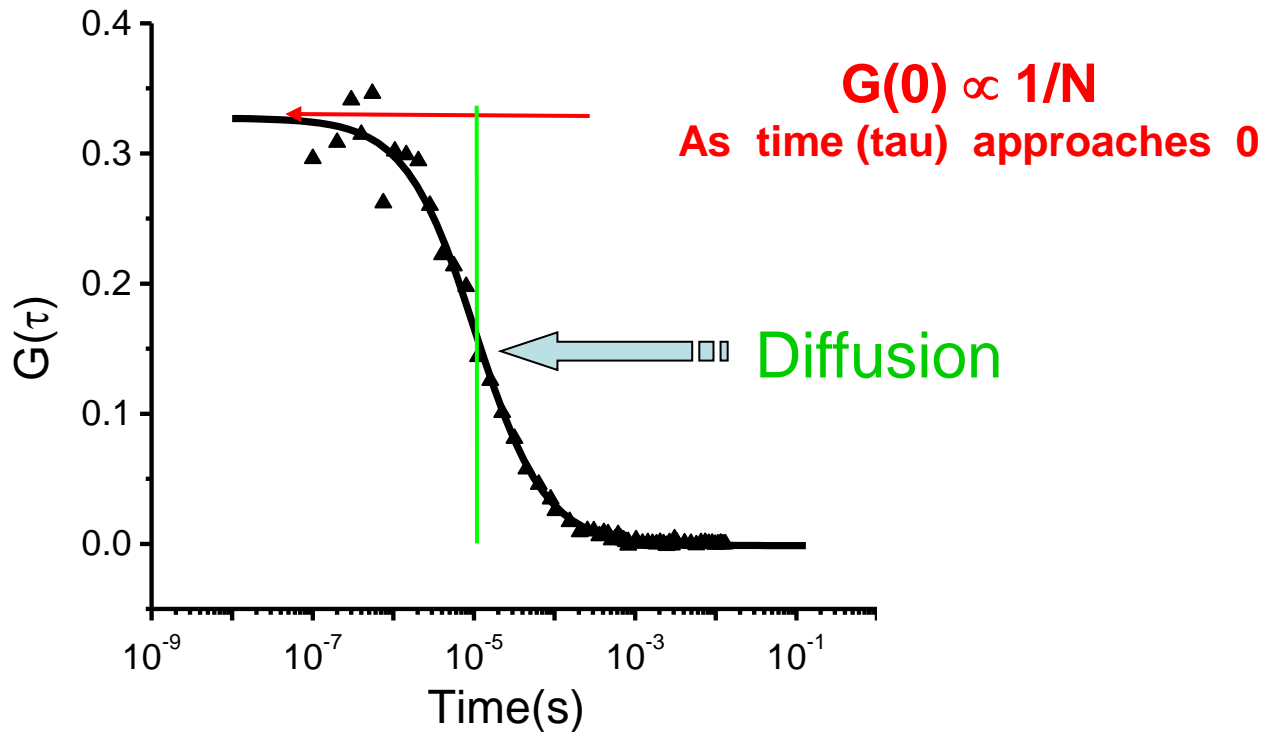
Volume:  $10^{-15}$  L

Size ( $\mu\text{m}$ ):  $0.3 \times 1$

No. of molecules:  $\approx 1$



# The Autocorrelation Function

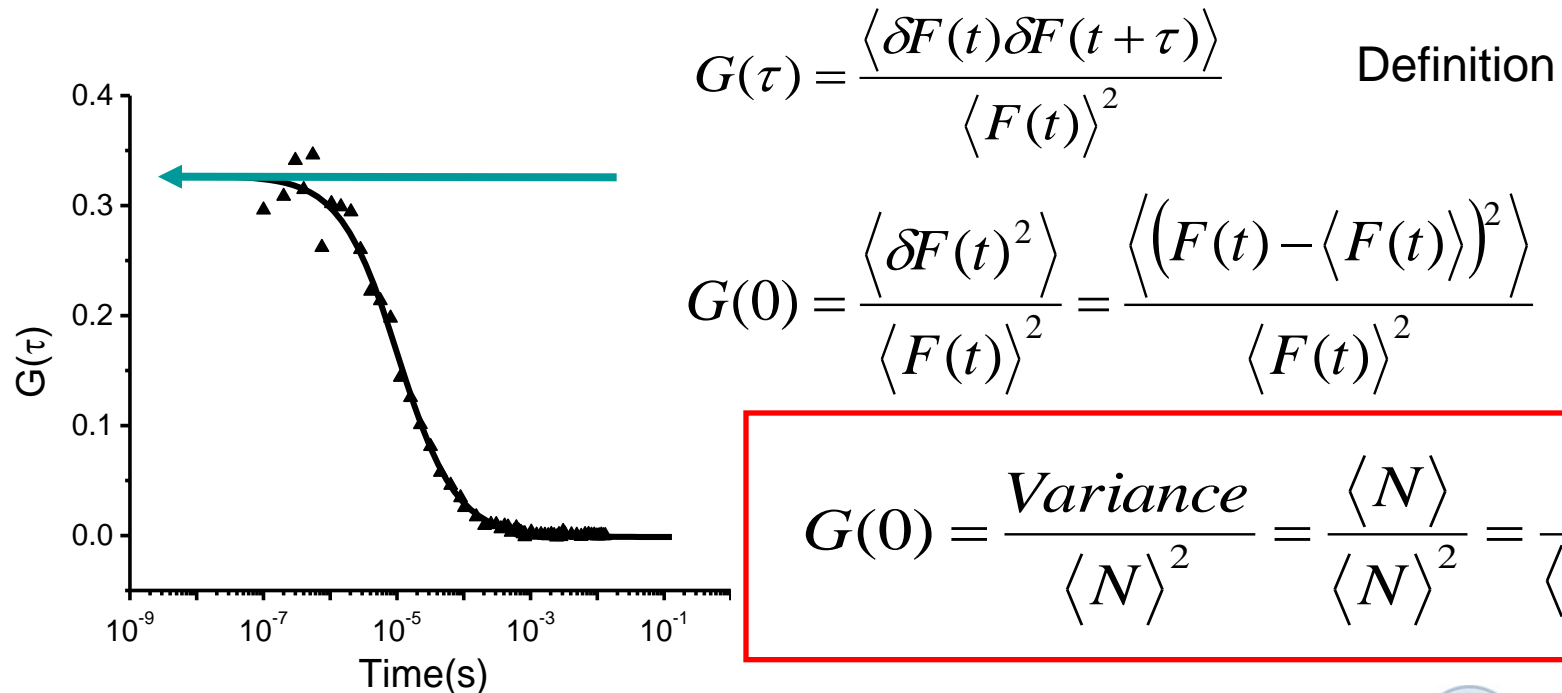


In the simplest case, two parameters define the autocorrelation function: the amplitude of the fluctuation ( $G(0)$ ) and the characteristic relaxation time of the fluctuation

# Why Is $G(0)$ Proportional to $1/\text{Particle Number}$ ?

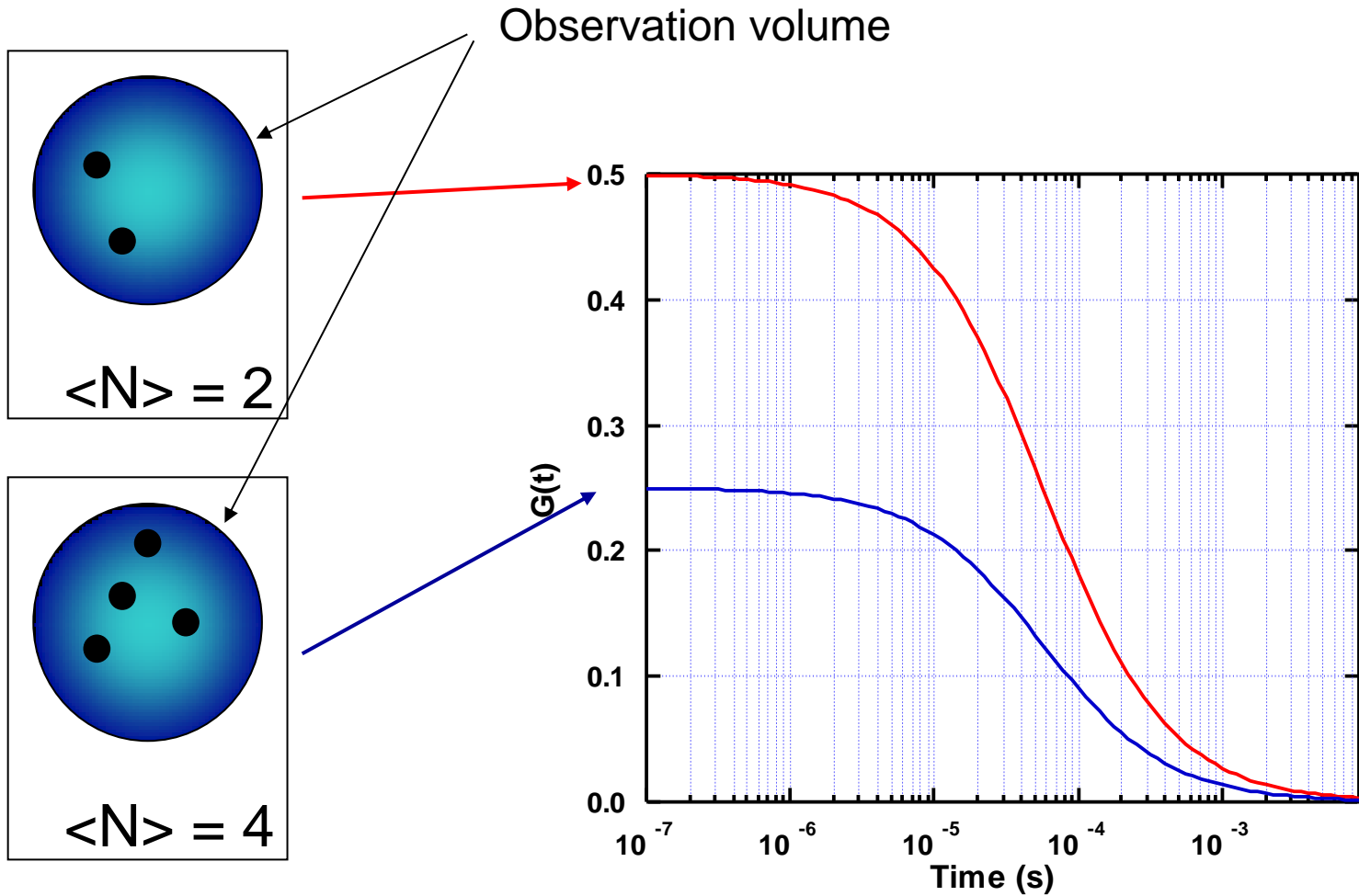
A Poisson distribution describes the statistics of particle occupancy fluctuations. For a Poisson distribution the variance is proportional to the average:

$$\langle N \rangle = \langle \text{Particle Number} \rangle = \text{Variance}$$



$$G(0) = \frac{\text{Variance}}{\langle N \rangle^2} = \frac{\langle N \rangle}{\langle N \rangle^2} = \frac{1}{\langle N \rangle}$$

# The Effects of Particle Concentration on the Autocorrelation Curve



# The Effects of Particle Size on the Autocorrelation Curve

## Diffusion Constants

300  $\mu\text{m}^2/\text{s}$

90  $\mu\text{m}^2/\text{s}$

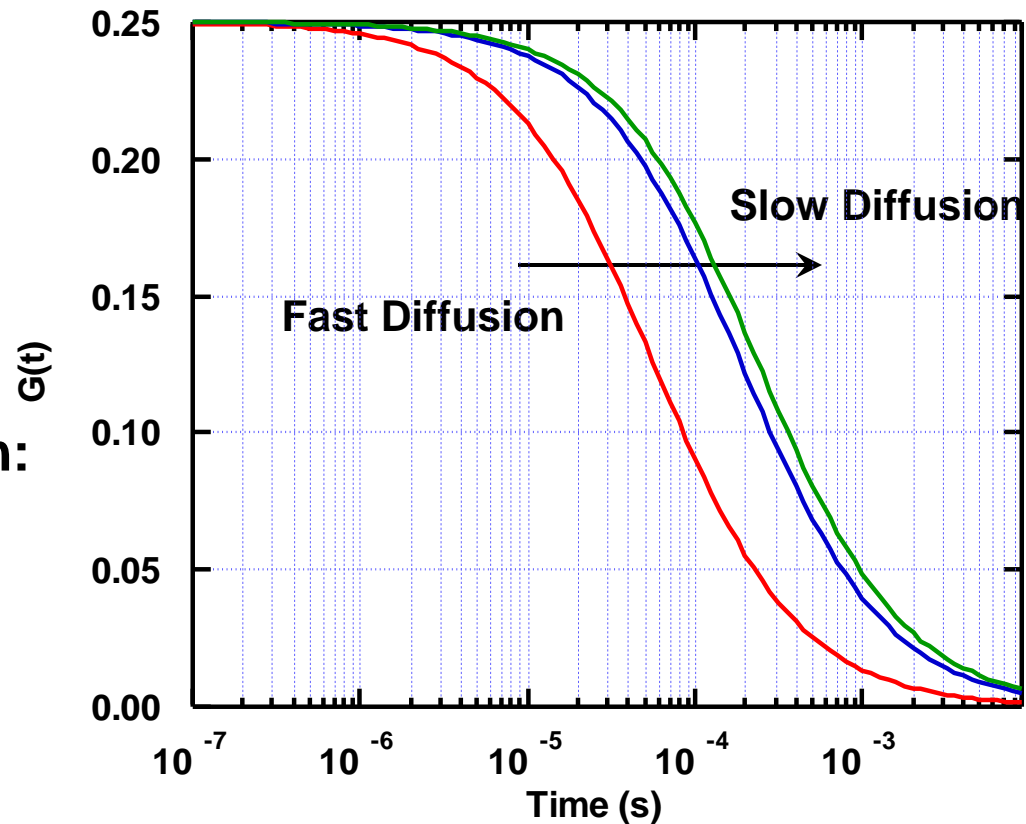
71  $\mu\text{m}^2/\text{s}$

## Stokes-Einstein Equation:

$$D = \frac{kT}{6\pi\eta r}$$

$$\langle x \rangle = \sqrt{6D} \sqrt{t}$$

$$MW \propto \text{Volume} \propto r^3$$



Monomer --> Dimer

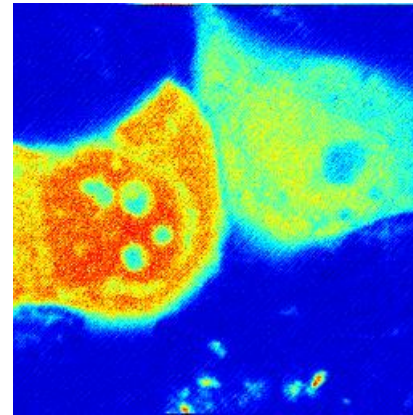
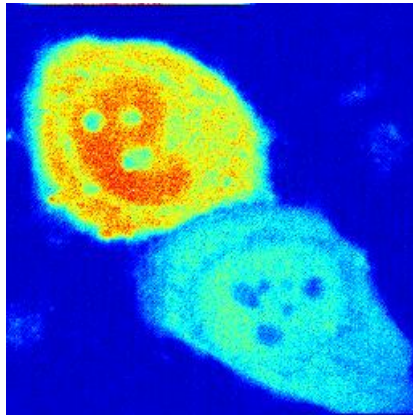
Only a change in D by a factor of  $2^{1/3}$ , or 1.26

# Table of characteristic times for diffusion

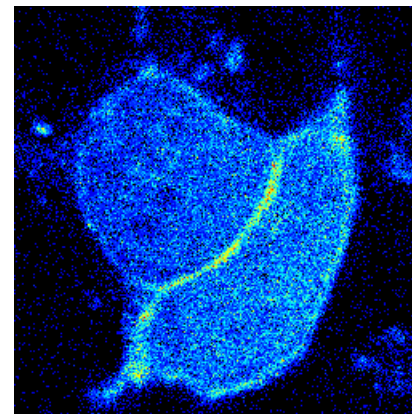
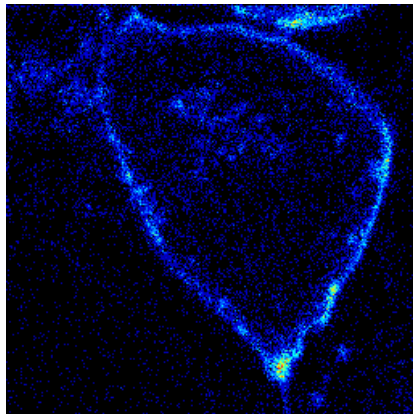
**Orders of magnitude** (for 1  $\mu\text{M}$  solution, small molecule, water)

<b>Volume</b>	<b>Device</b>	<b>Size(<math>\mu\text{m}</math>)</b>	<b>Molecules</b>	<b>Time</b>
milliliter	cuvette	10000	$6 \times 10^{14}$	$10^4$
microliter	plate well	1000	$6 \times 10^{11}$	$10^2$
nanoliter	microfabrication	100	$6 \times 10^8$	1
picoliter	typical cell	10	$6 \times 10^5$	$10^{-2}$
femtoliter	confocal volume	1	$6 \times 10^2$	$10^{-4}$
attoliter	nanofabrication	0.1	$6 \times 10^{-1}$	$10^{-6}$

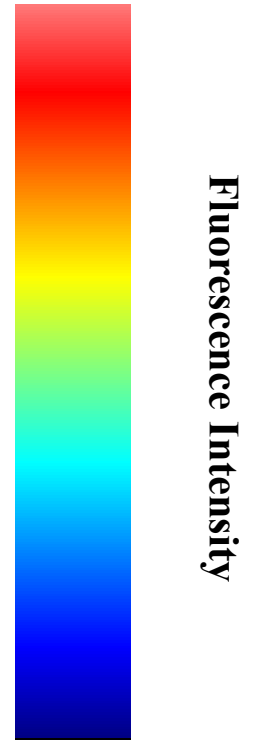
# Autocorrelation Adenylate Kinase -EGFP Chimeric Protein in HeLa Cells



Examples of different *HeLa* cells transfected with AK1-EGFP

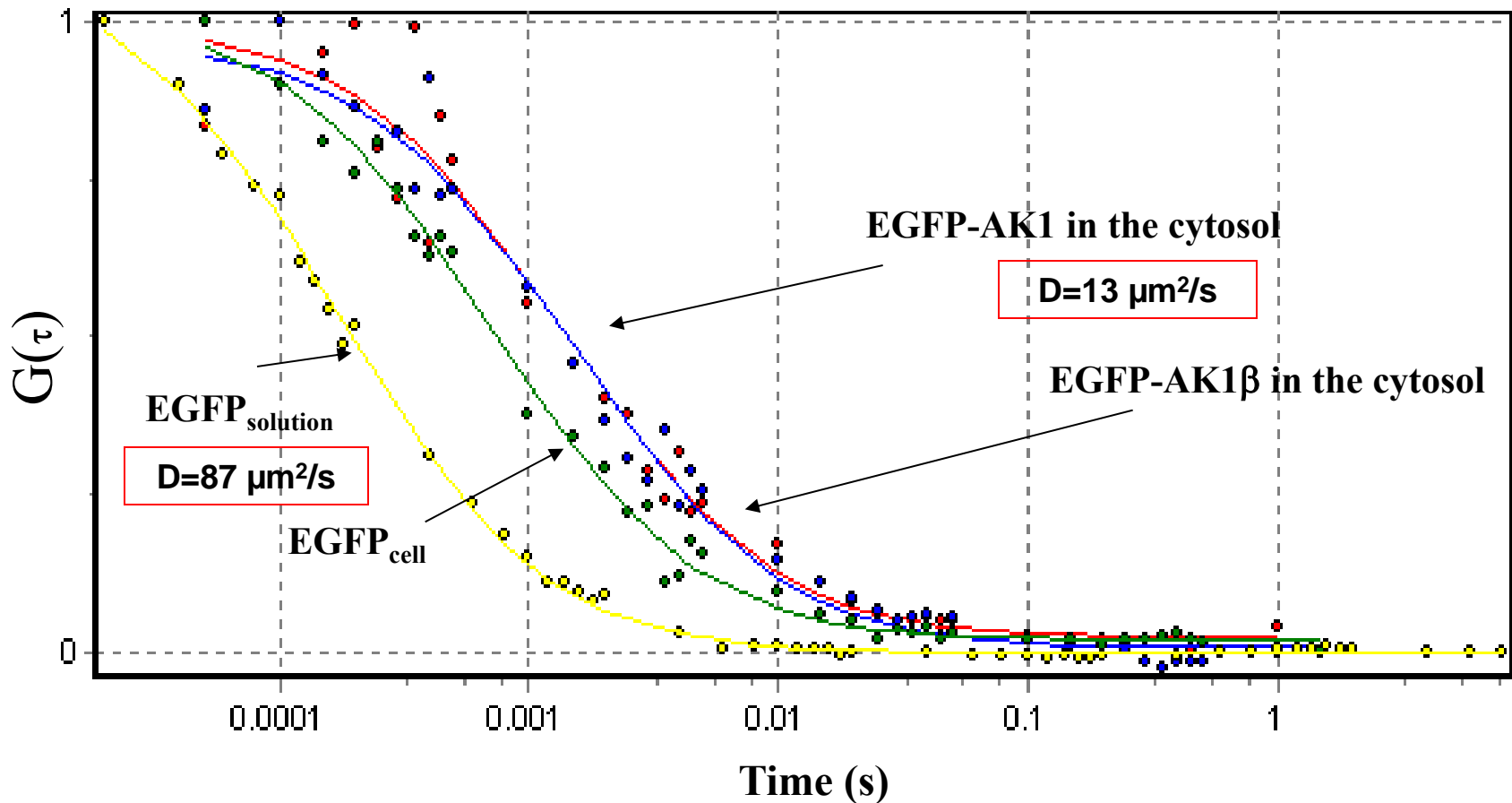


Examples of different *HeLa* cells transfected with AK1 $\beta$  -EGFP



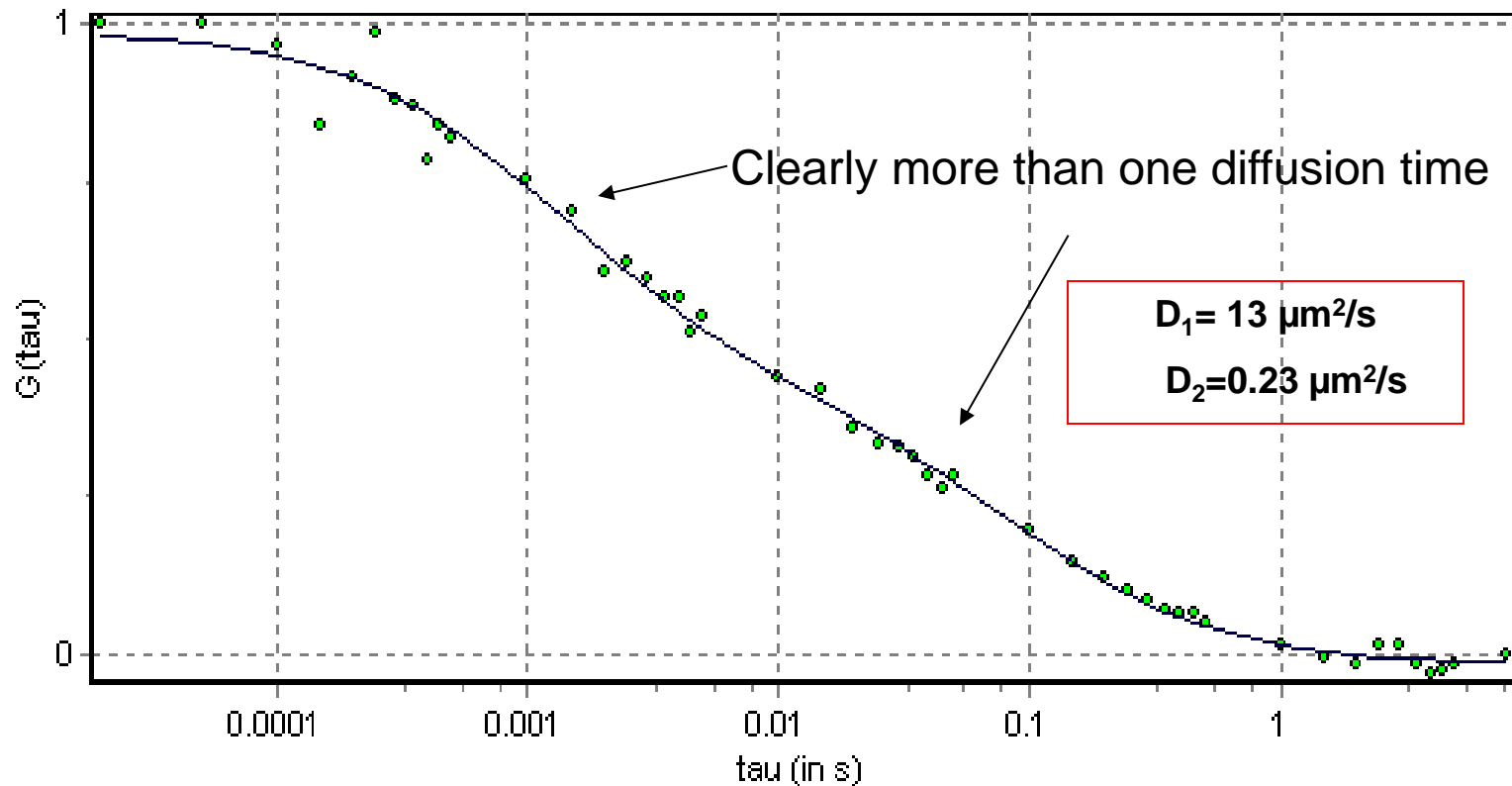


# Autocorrelation of EGFP & Adenylate Kinase -EGFP



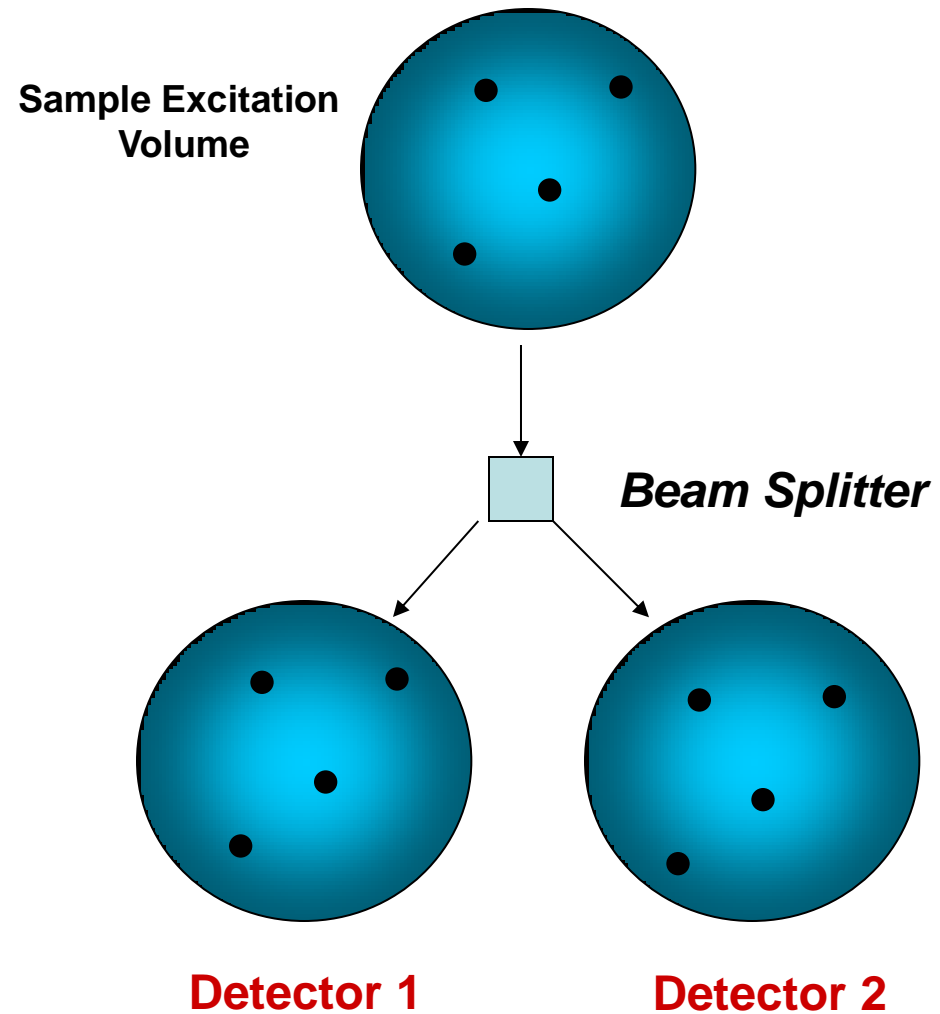
Normalized autocorrelation curve of EGFP in solution ( $\bullet$ ), EGFP in the cell ( $\bullet$ ), AK1-EGFP in the cell( $\bullet$ ), AK1 $\beta$ -EGFP in the cytoplasm of the cell( $\bullet$ ).

# Autocorrelation of Adenylate Kinase –EGFP on the Membrane



A mixture of AK1 $\beta$ -EGFP in the plasma membrane of the cell.

# Two Channel Detection: Cross-correlation

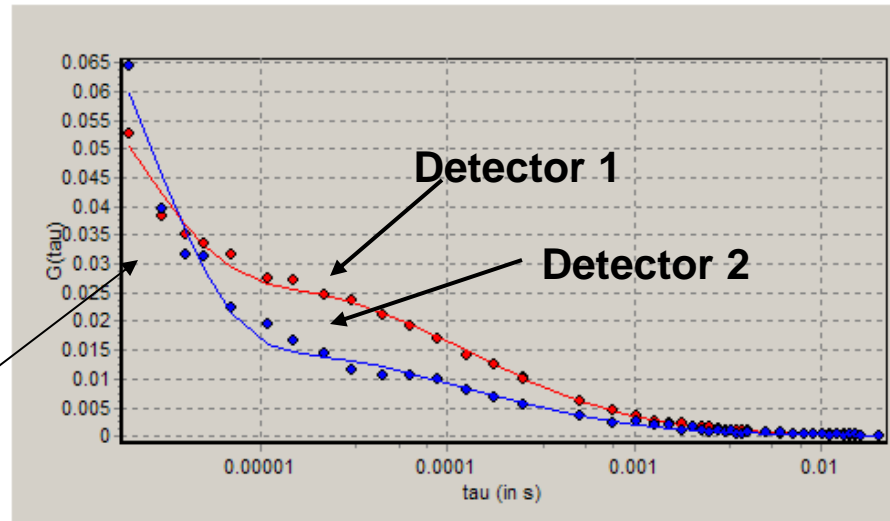


1. Increases signal to noise by isolating correlated signals.
2. Corrects for PMT noise

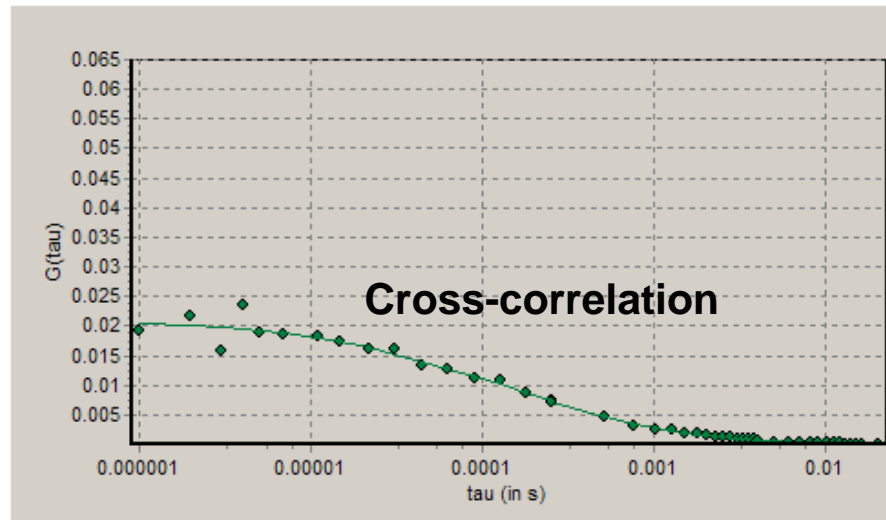
Each detector observes  
the same particles

# Removal of Detector Noise by Cross-correlation

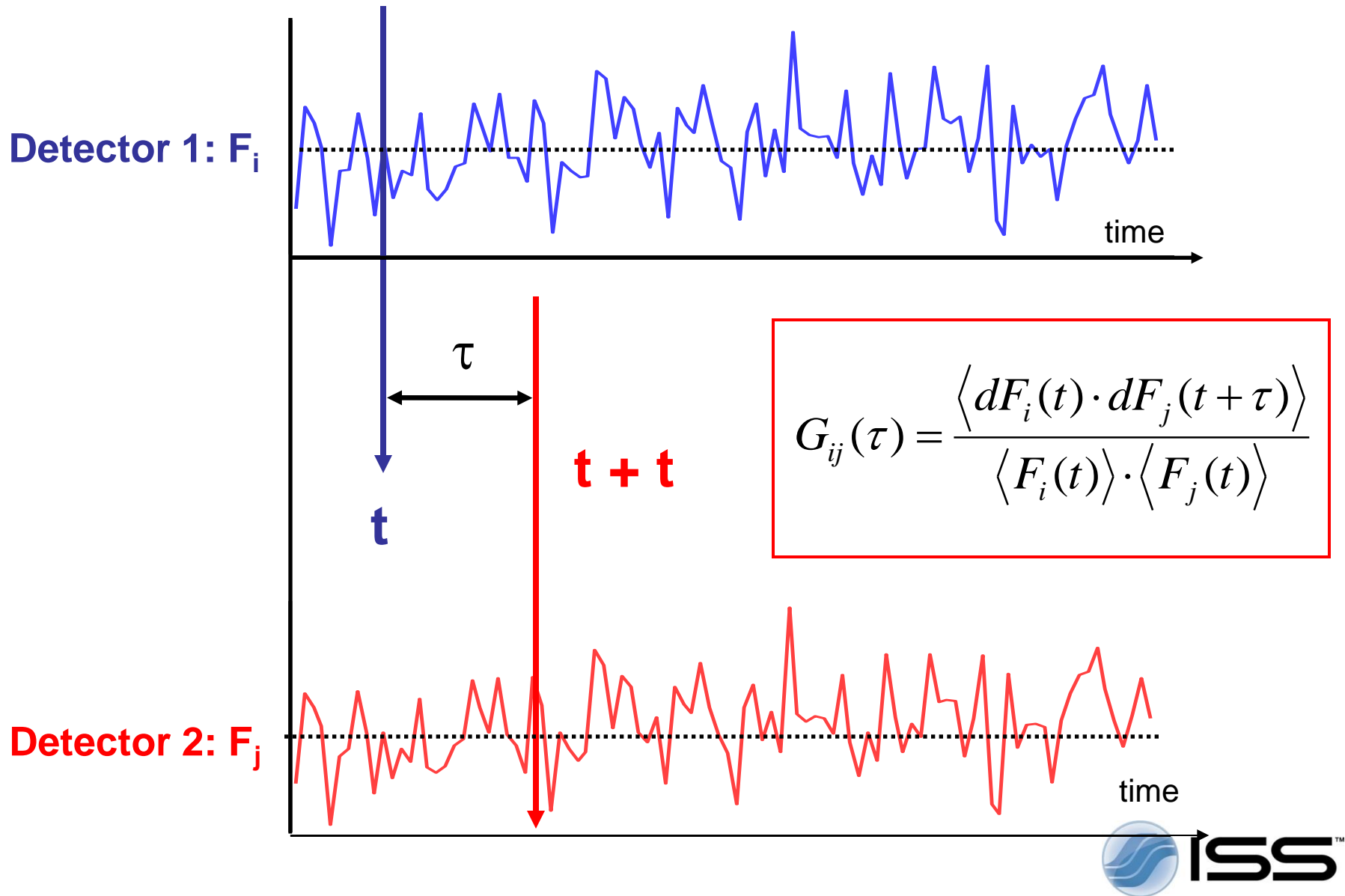
11.5 nM Fluorescein



Detector after-pulsing



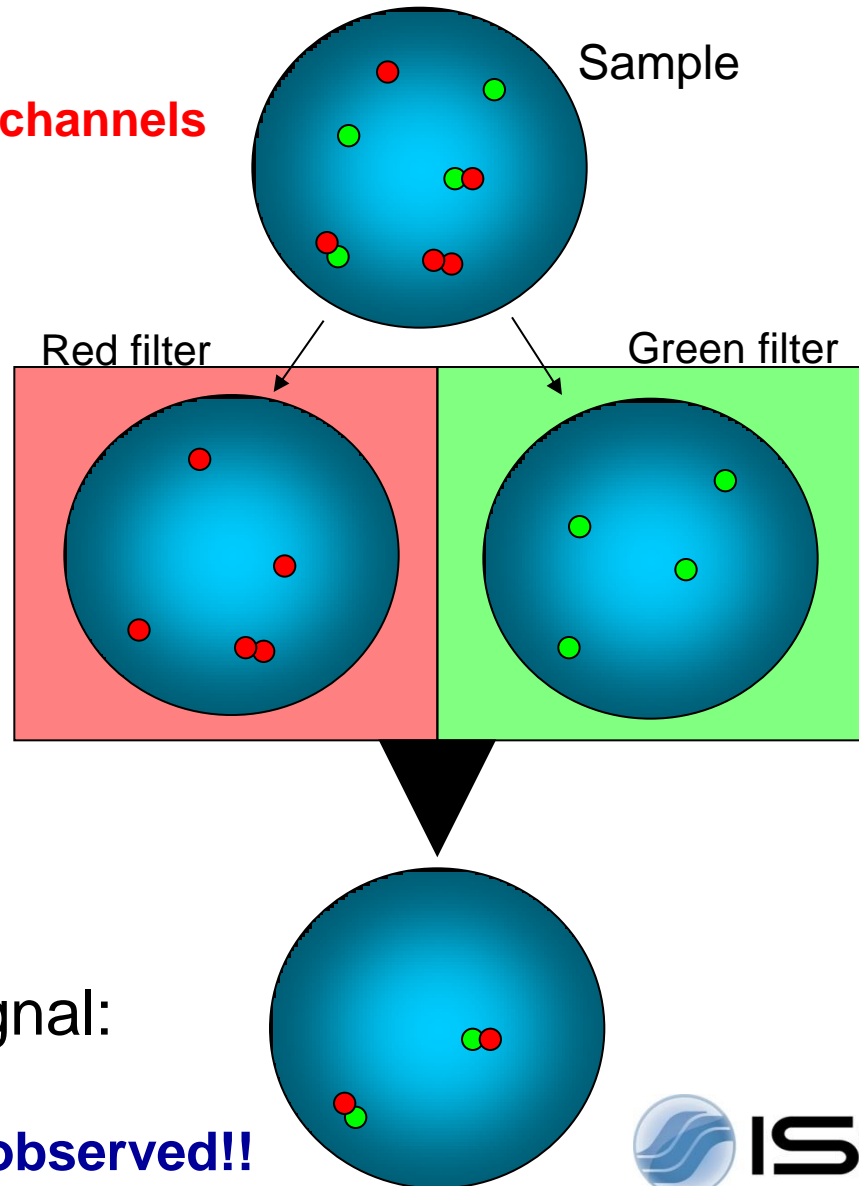
# Calculating the Cross-correlation Function



# Two-Color Cross-correlation

**The cross-correlation  
ONLY if particles are observed in both channels**

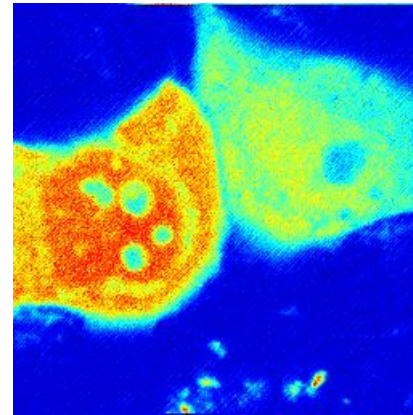
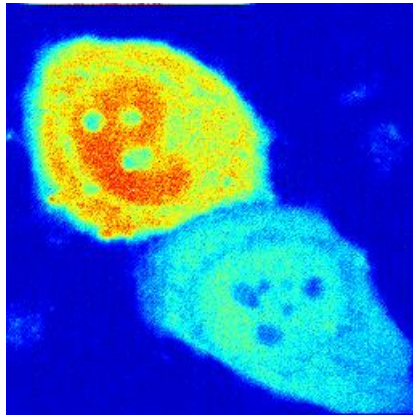
Each detector observes  
particles with a particular color



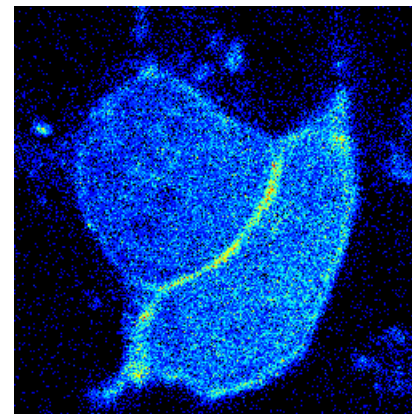
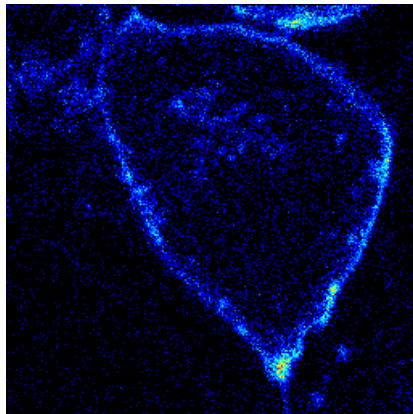
The cross-correlation signal:

**Only the green-red molecules are observed!!**

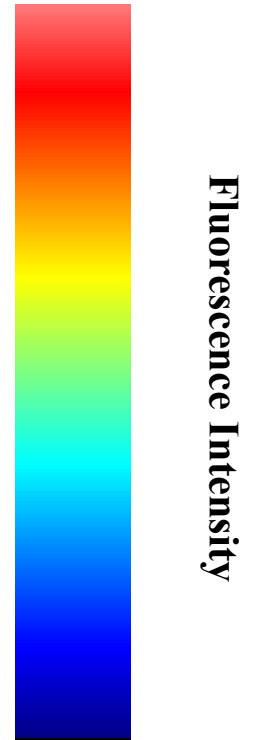
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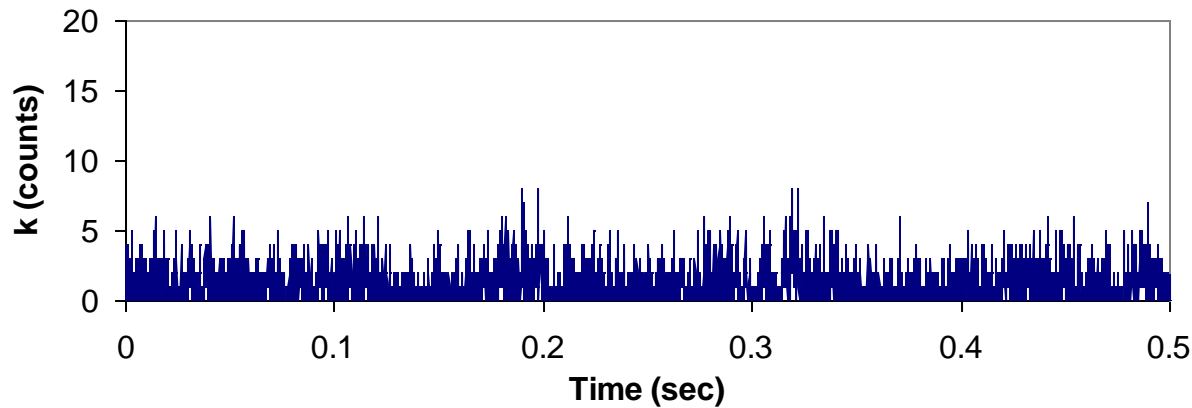
Examples of different *HeLa* cells transfected with AK1-EGFP



Examples of different *HeLa* cells transfected with AK1 $\beta$  -EGFP

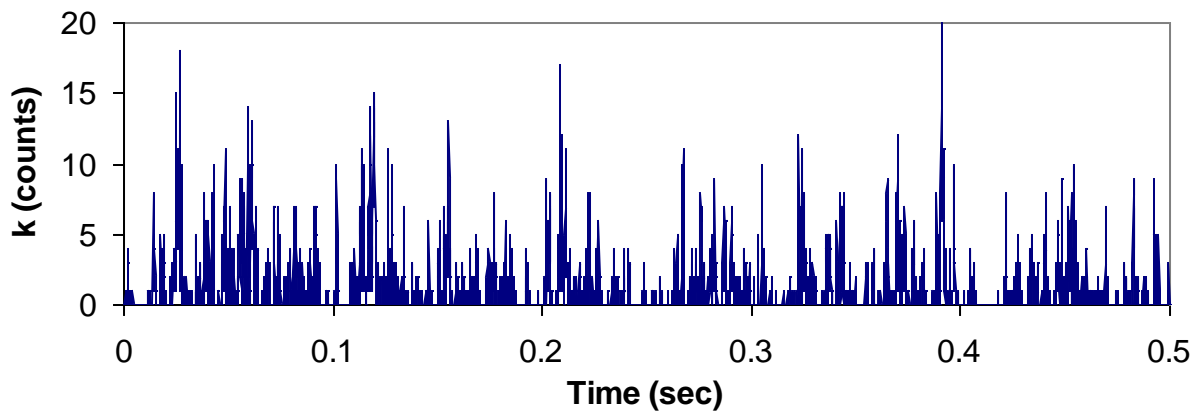


# Fluorescence Trajectories



Fluorescent  
Monomer:

Intensity = 115,000 cps

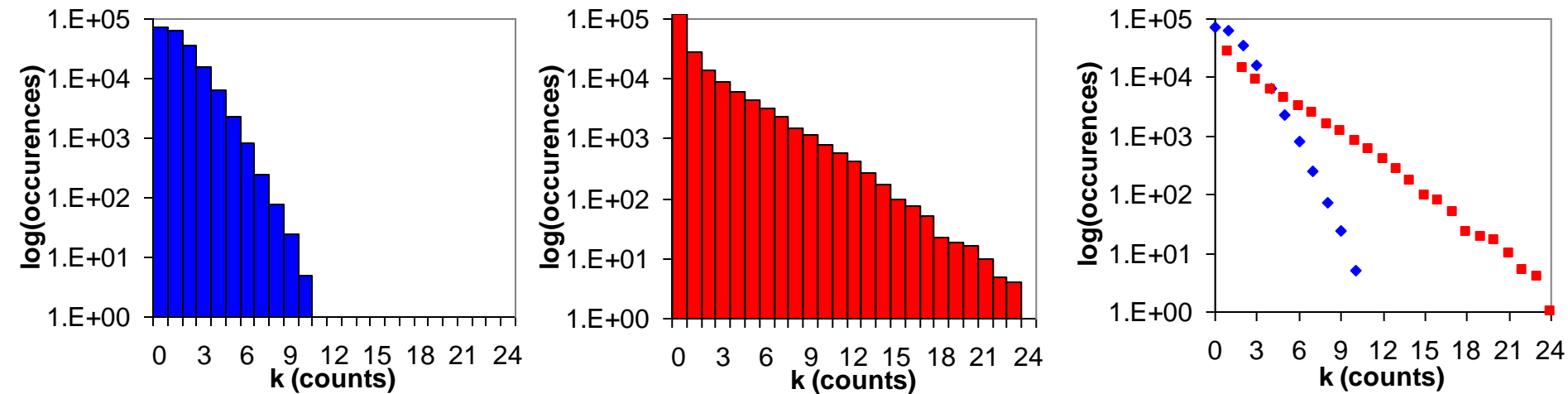


Aggregate:

Intensity = 111,000 cps



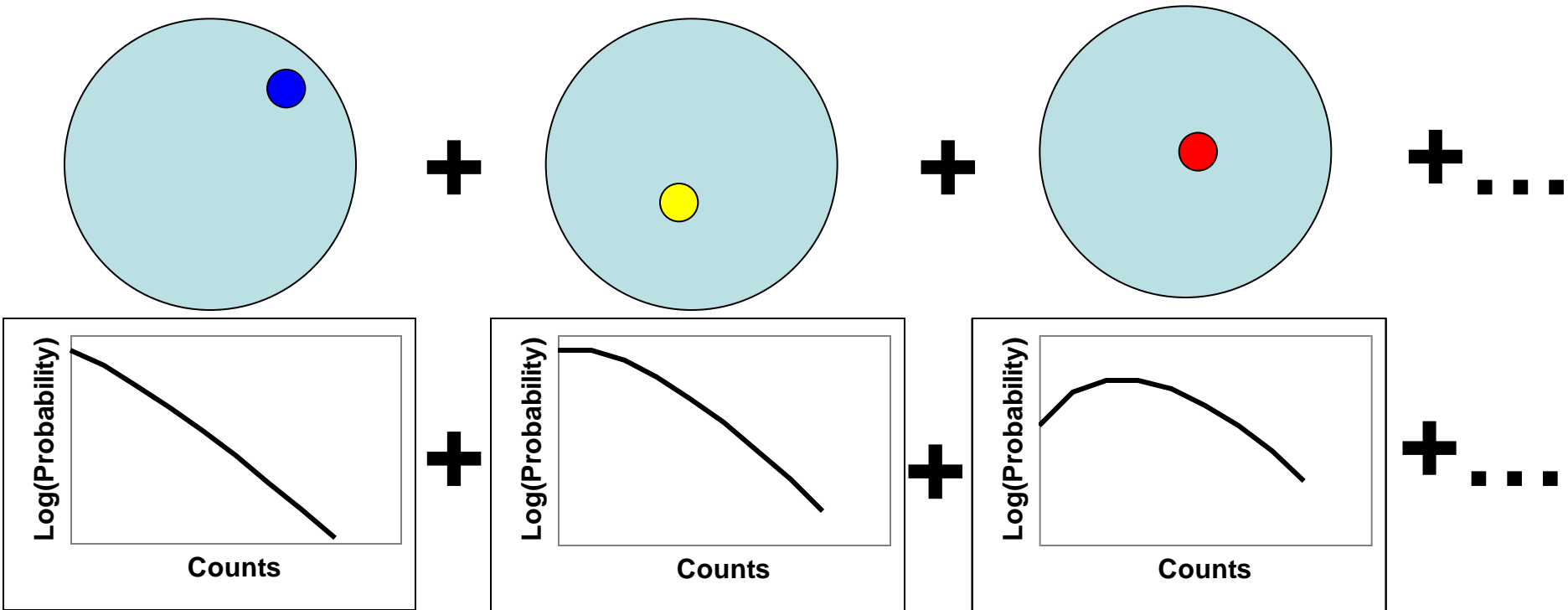
# Photon Count Histogram (PCH)



Can we quantitate this?

What contributes to the distribution of intensities?

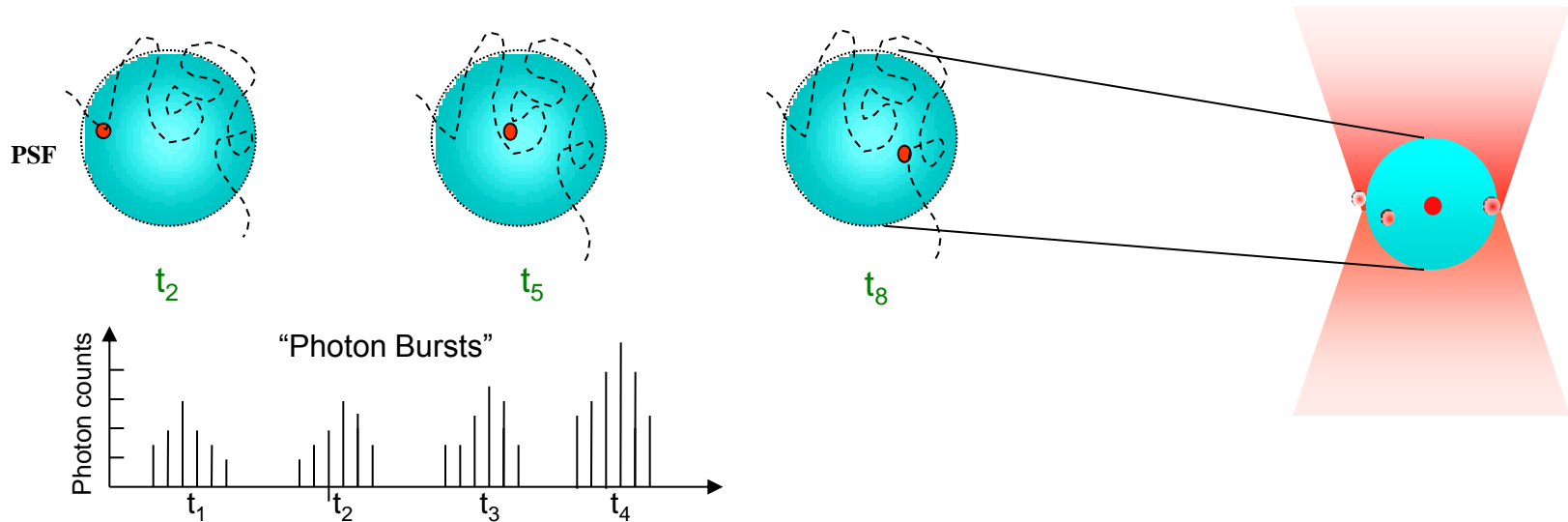
# Single Particle PCH



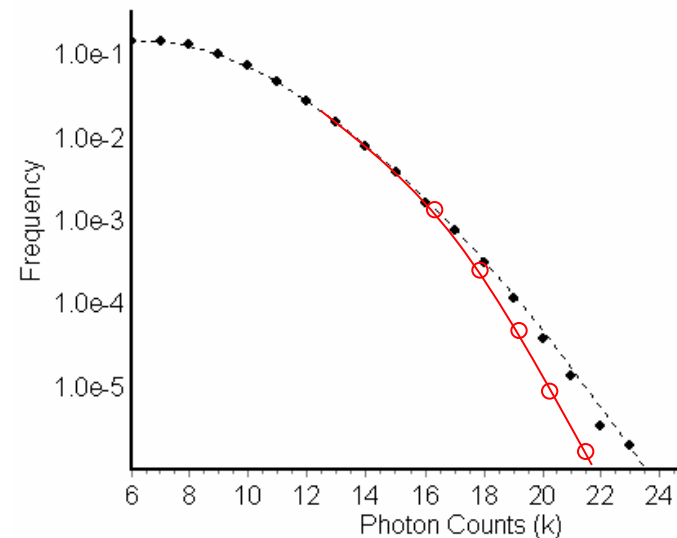
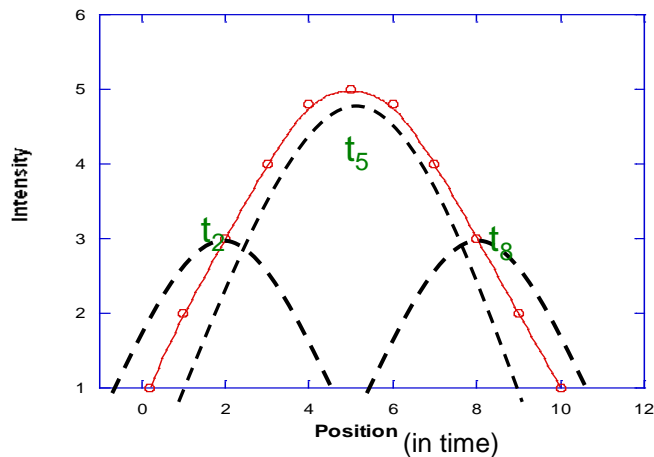
Have to sum up the poissonian distributions for all possible positions of the particle within the PSF

$$p^{(1)}(k) = \frac{1}{V_0} \int_{V_0} Poi(k, \overline{\varepsilon PSF(\vec{r})}) d\vec{r}$$

# The average photon count rate of bursts determines the molecular brightness of the labeled protein



The intensity distribution accounts for the fluctuations of photons from the molecule freely diffusing through the excitation profile. Thus, the overall photon counting count distribution is the weighted superposition of individual Poissonian distributions for each intensity values with a scaling amplitude. The fluctuations light intensity results in a broadening of photon count distribution with respect to a pure poisson distribution. As the fluctuations increases, the photon count distribution broadens.



# Multiple-Particle PCH

- What if I have two particles in the PSF?
- Have to calculate every possible position of the second particle for each possible position of the first!

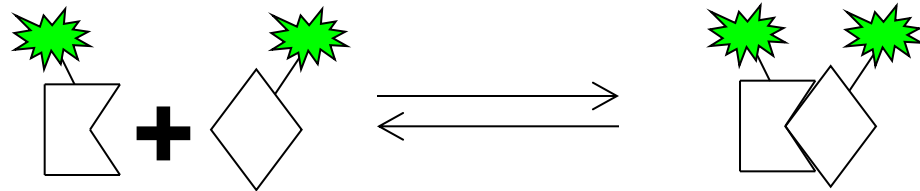
# The Photon Counting Histogram: Statistical Analysis of Single Molecule Populations

- The Autocorrelation function only depends on fluctuation duration and fluctuation density (independent of excitation power)
- PCH: distribution of intensities (independent of time)

# Hypothetical situation: Protein Interactions

- 2 proteins are labeled with a fluorophore
- Proteins are soluble
- How do we assess interactions between these proteins?

# Dimer has double the brightness



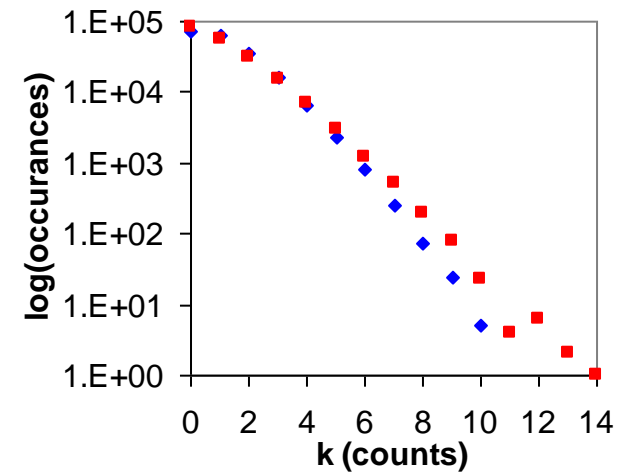
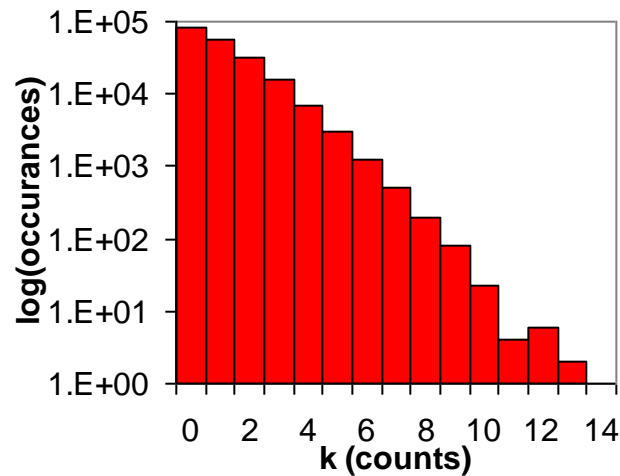
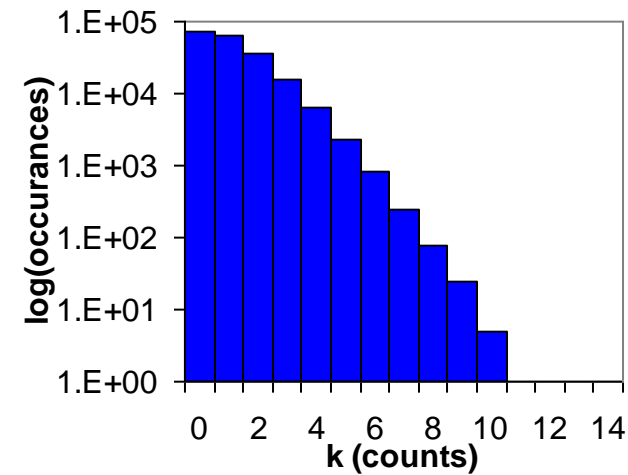
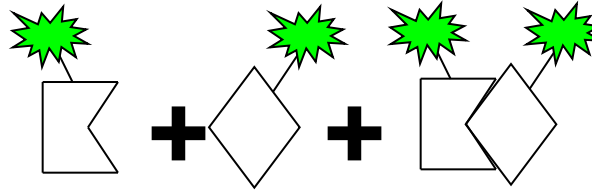
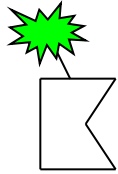
$$\varepsilon = \varepsilon_{monomer}$$

$$\varepsilon = 2 \times \varepsilon_{monomer}$$

All three species are present in  
equilibrium mixture

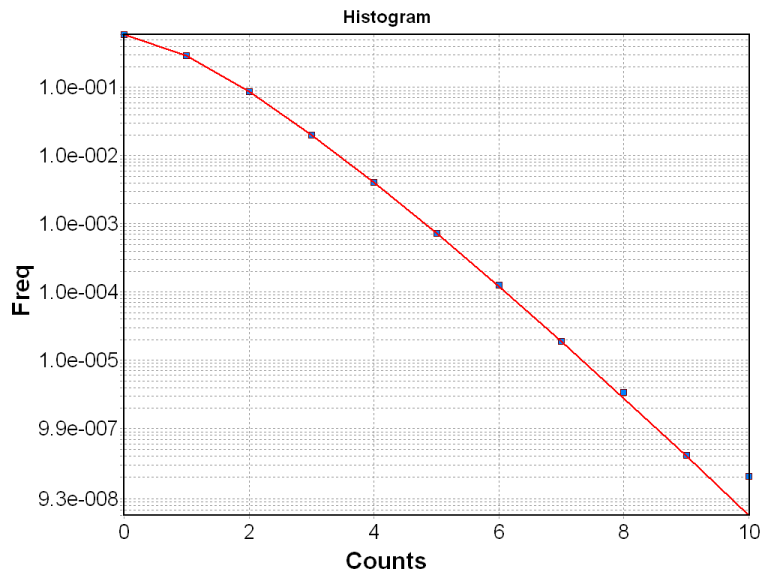
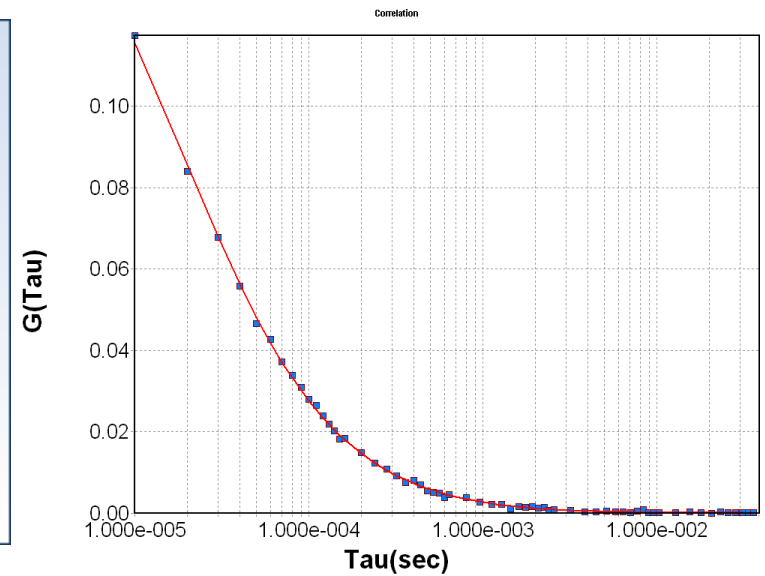
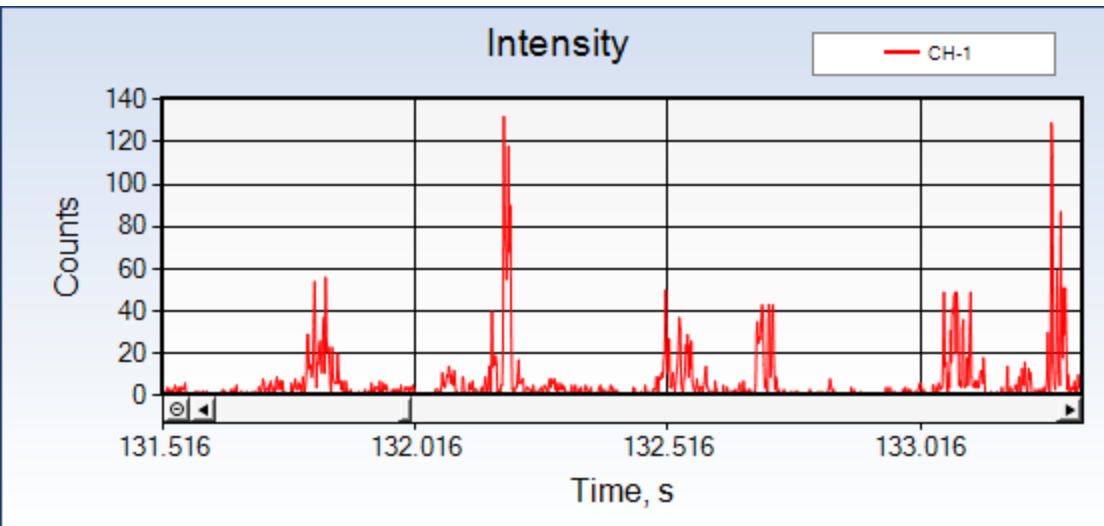
Typical one photon  $\varepsilon_{monomer} = 10,000$  cpsm

# Photon Count Histogram (PCH)





# Data Presentation and Analysis



*FCS parameters:*  $\langle N \rangle$  and  $D$

*PCH parameters:*  $\langle N \rangle$  and  $\epsilon$

$\langle N \rangle$ : no. of particles in the observation volume

$D$ : diffusion coefficient

$\epsilon$ : brightness

# Complementary information obtained with the same measurement

## using Autocorrelation function (FCS):

- ✓ Diffusion Coefficient (diffusion times)
- ✓ No. of particles in observation volume

## using Photon Counting Histogram (PCH) analysis:

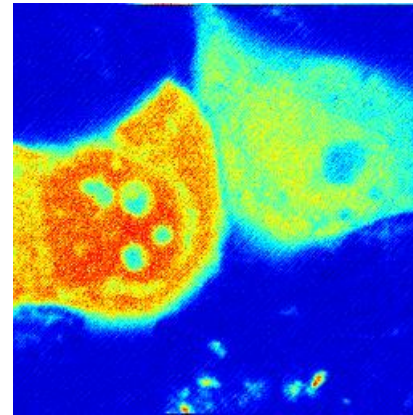
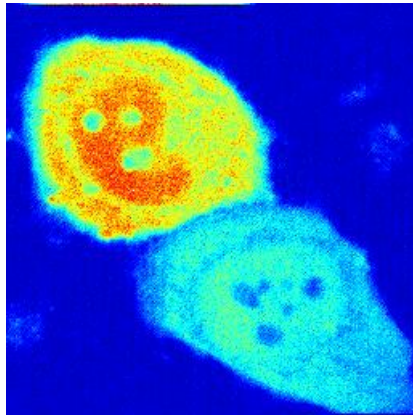
- ✓ Brightness
- ✓ No. of particles in observation volume

- The Autocorrelation function only depends on fluctuation duration and fluctuation density (independent of excitation power)
- PCH: distribution of intensities (independent of time)

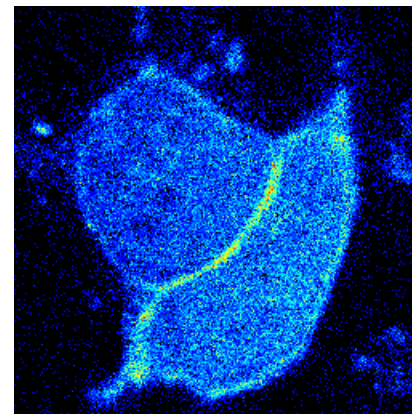
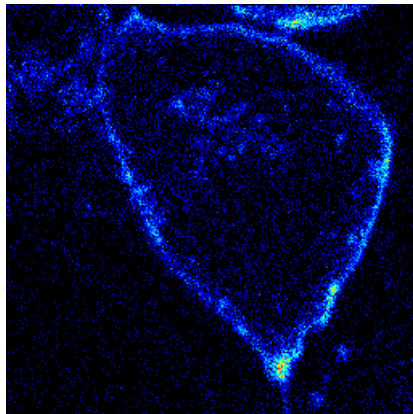
# What about ... ?

- In a cell we may want to locate the areas where we have clusters of molecules versus single molecules.
- In cells, both the concentration and the clustering of proteins can differ in various locations and change during biological processes.
- Number & Brightness (N&B) measures the average number of molecules and brightness in each pixel of an image.

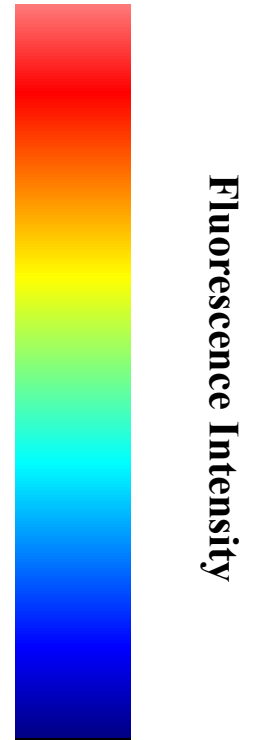
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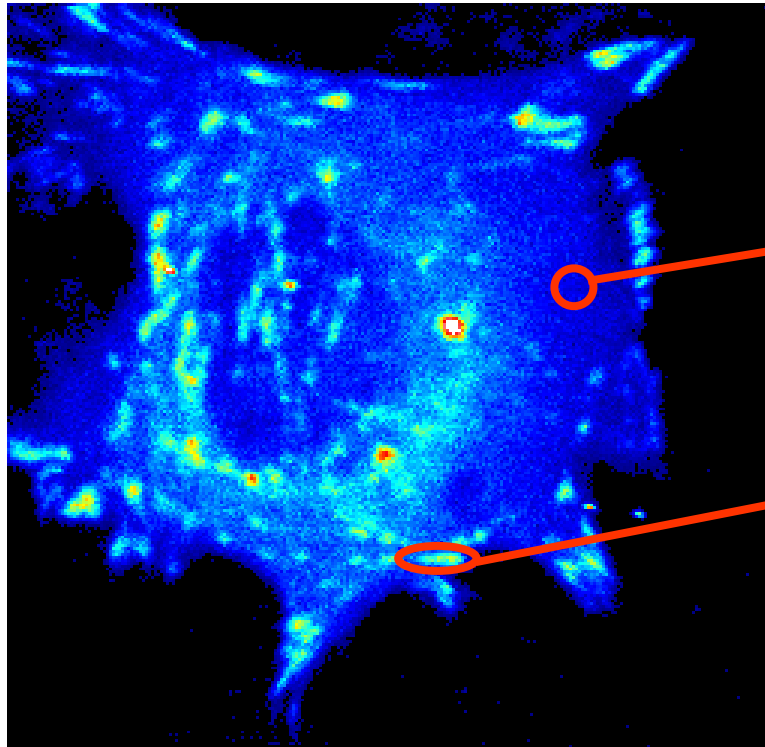


# Existing Methods to determine protein concentration and aggregation of proteins in cells

- Calibrate the fluorescence intensity
- FRET
- ICS, Image Correlation Spectroscopy
- PCH

# Intensity

## 1. Calibration of the free fluorophore based on intensity



Average intensity of MEF cells  
expressing Paxillin-EGFP

**A** INTENSITY  
31,250 counts/sec

**B**  
93,750 counts/sec

If “free” EGFP at 10nM gave 30,000  
counts/sec then the conclusion would  
be that :

**A** = 10nM

**B** = 30nM

However, it doesn't give you the size distribution  
Only concentration is given

# The Number and Brightness (N&B) analysis

**Purpose:** Provide a pixel resolution map of molecular number and aggregation in cells

**Method:** First and second moment of the fluorescence intensity distribution at each pixel

**Source:** Raster scanned image obtained with laser scanning microscopes  
TIRF with fast cameras  
Spinning disk confocal microscope

**Output:** The N and B maps, B vs intensity 2D histogram

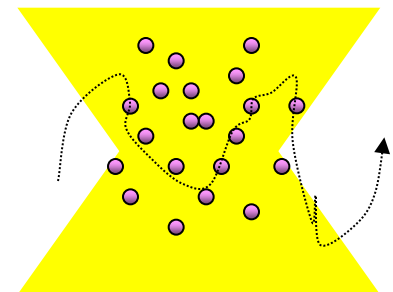
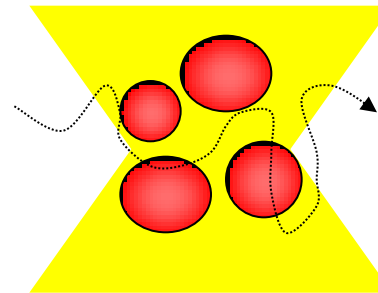
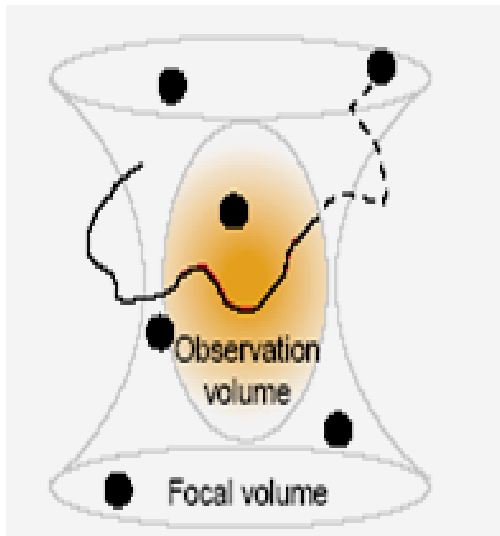
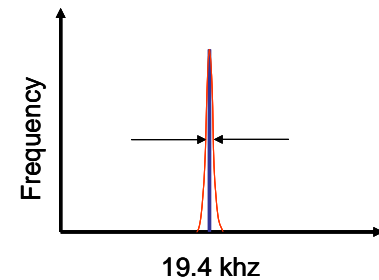
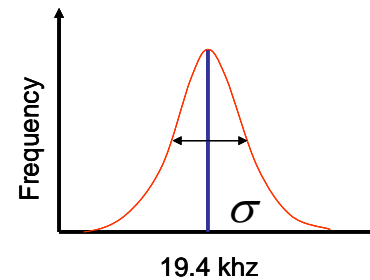
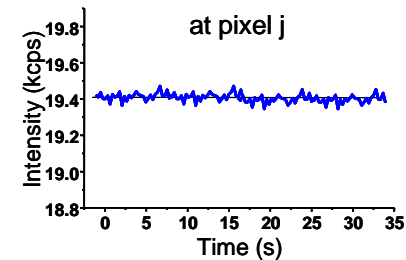
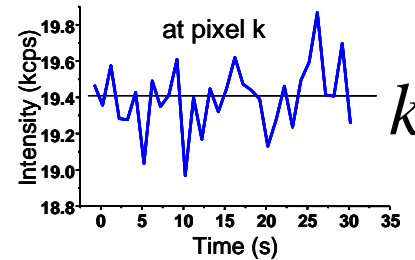
# How to distinguish pixels with many dim molecules from pixels with few bright molecules?

Average  
(first moment)

$$\langle k \rangle = \frac{\sum_i k_i}{K}$$

Variance  
(second moment)

$$\sigma^2 = \frac{\sum_i (k_i - \langle k \rangle)^2}{K}$$



- Given two series of equal average, the larger is the variance, the less molecules contribute to the average. The ratio of the square of the average intensity ( $\langle k \rangle^2$ ) to the variance ( $\sigma^2$ ) is proportional to the average number of particles  $\langle N \rangle$ .

$$G(0) = \sigma^2 / \langle k \rangle^2 = 1/N$$





# Calculating protein aggregates from images

This analysis provides a map of  $\langle N \rangle$  and brightness (B) for every pixel in the image. The units of brightness are related to the pixel dwell time and they are “counts/dwell time/molecule”.

$$\langle k \rangle = \frac{\sum_i k_i}{K} \quad \sigma^2 = \frac{\sum_i (k_i - \langle k \rangle)^2}{K}$$

$$\langle N \rangle = \frac{\langle k \rangle^2}{\sigma^2}$$

$$B = \frac{\langle k \rangle}{\langle N \rangle} = \frac{\sigma^2}{\langle k \rangle}$$

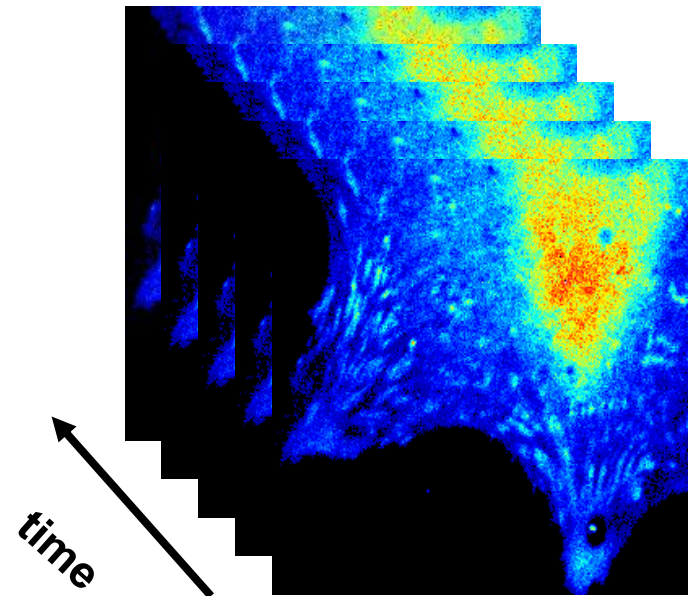
$\sigma^2$  = Variance

$\langle k \rangle$  = Average counts

N = Apparent number of molecules

B = Apparent molecular brightness

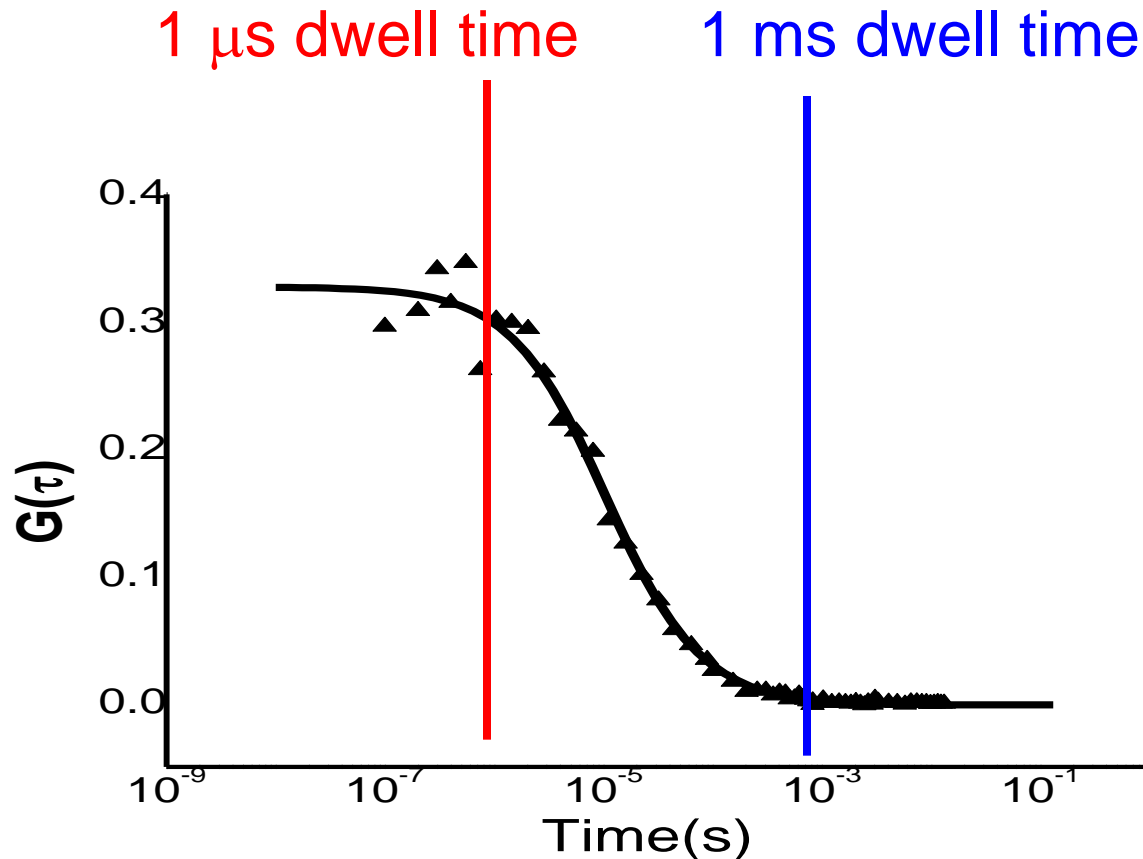
K = # of frames analyzed



# Selecting the dwell time

To increase the apparent brightness we could increase the dwell time, since the brightness is measured in counts/dwell time/molecule.

Increasing the dwell time decreases the amplitude of the fluctuation.



# What contributes to the variance?

The measured variance contains two terms, the variance due to the particle number fluctuation and the variance due to the detector count statistics noise

$$\sigma^2 = \sigma_n^2 + \sigma_d^2$$

Variance due to particle number fluctuations  $\sigma_n^2 = \varepsilon^2 n$

Variance due to detector shot noise  $\sigma_d^2 = \varepsilon n$  (for the photon counting detector)

Both depend on the intrinsic brightness and the number of molecules.

We can invert the equations and obtain  $n$  and  $\varepsilon$

$n$  is the true number of molecules

$\varepsilon$  is the true molecular brightness

## How to Calculate n and $\varepsilon$

$$B = \frac{\sigma^2}{\langle k \rangle} = \frac{\sigma_n^2}{\langle k \rangle} + \frac{\sigma_d^2}{\langle k \rangle} = \frac{\varepsilon^2 n}{\varepsilon n} + \frac{\sigma_d^2}{\langle k \rangle} = \varepsilon + 1$$

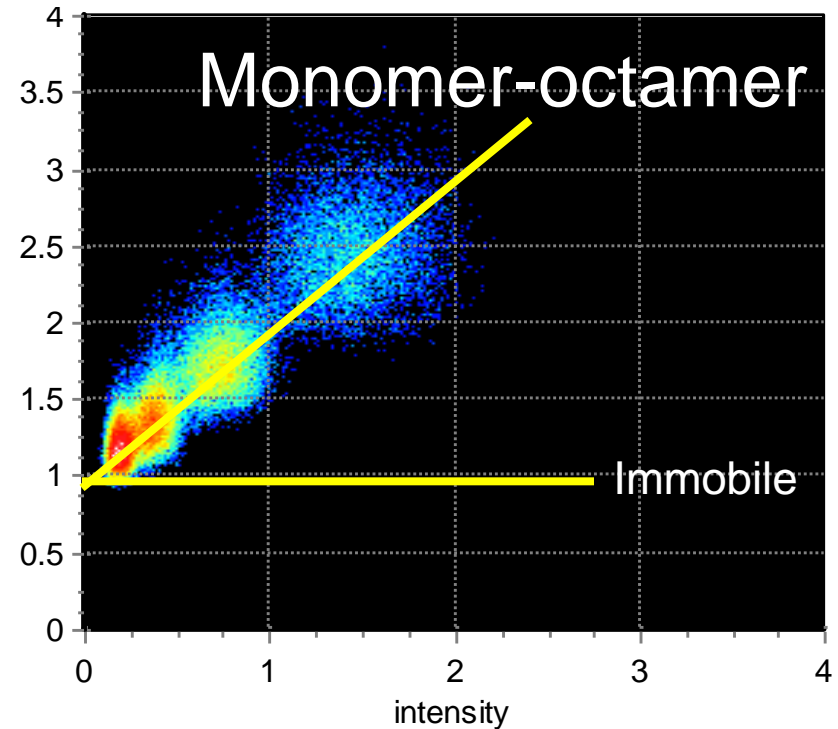
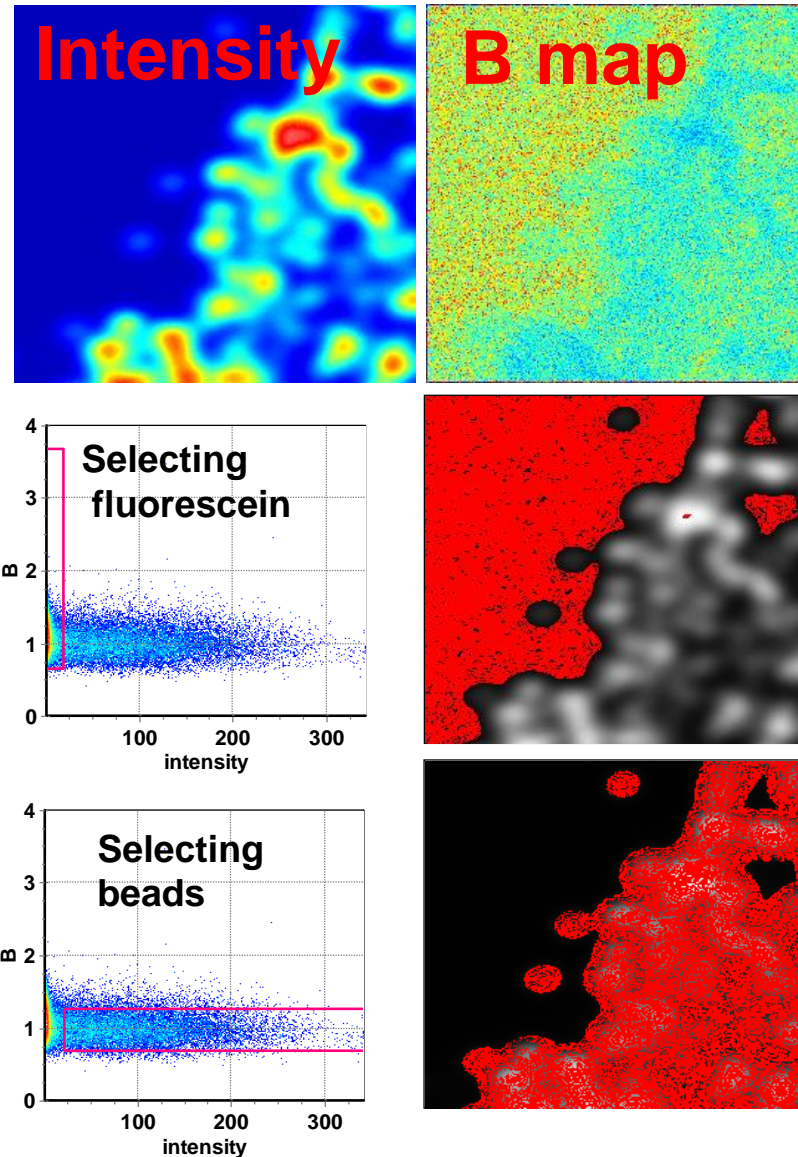
This ratio identifies pixels of different brightness due to mobile particles.

The “true” number of molecules n and the “true” molecular brightness for mobile particles can be obtained from

$$n = \frac{\langle k \rangle^2}{\sigma^2 - \langle k \rangle} \qquad \varepsilon = \frac{\sigma^2 - \langle k \rangle}{\langle k \rangle}$$

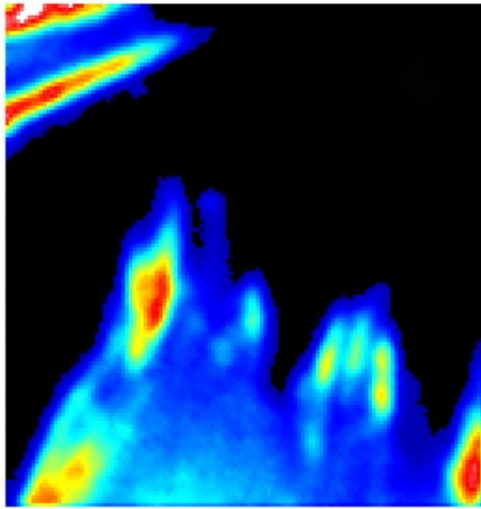
If there are regions of immobile particles, n cannot be calculated because for the immobile fraction the variance is =  $\langle k \rangle$ . For this reason, several plots are offered to help the operator to identify regions of mobile and immobile particles. Particularly useful is the plot of N vs B.

# The effect of the immobile part: with photon counting detectors (Fluorescent beads in a sea of 100nM Fluorescein).

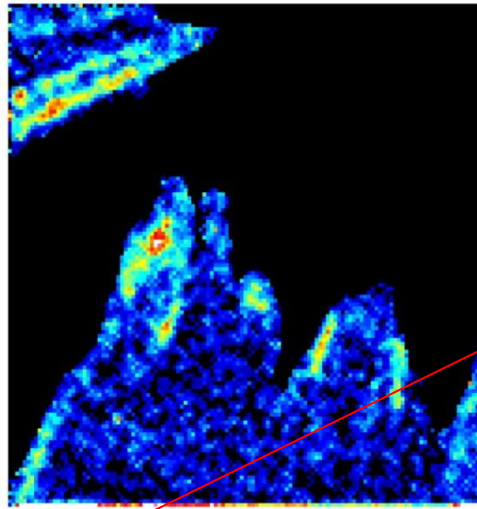


# Paxillin assembles as monomers and disassembles as aggregates as large as 8-12

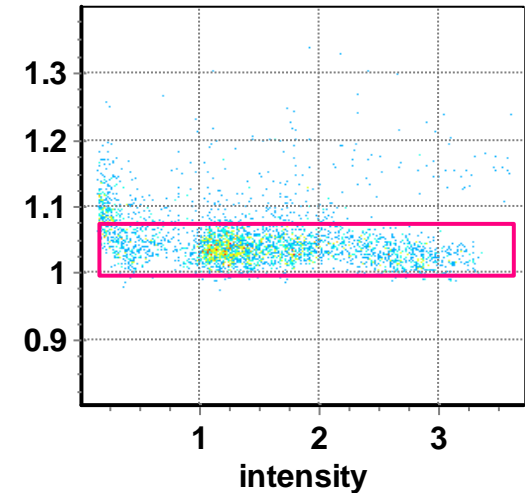
Average intensity



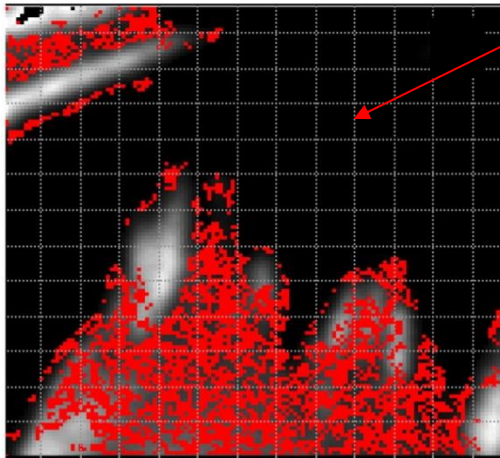
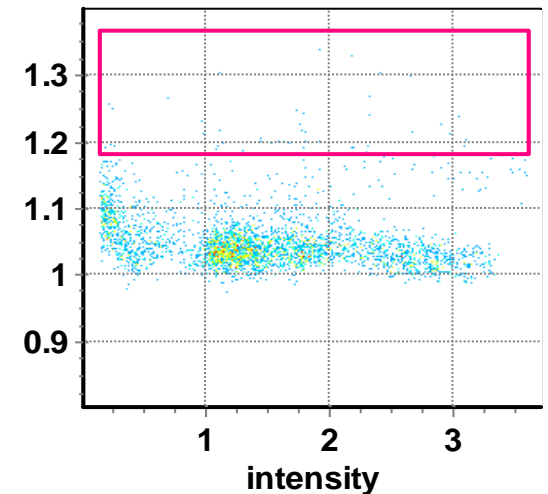
Molecular Brightness



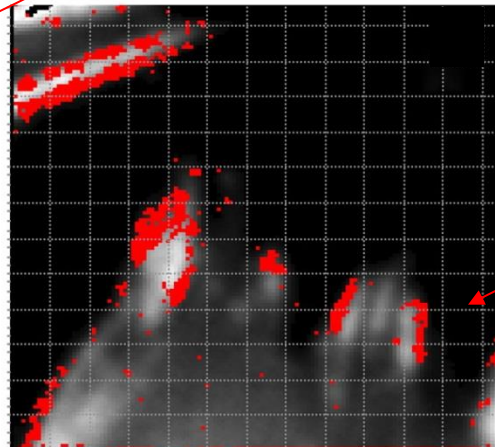
x= 1.90057 y= 1.03400 #pixels= 5702 in= 662



x= 1.88378 y= 1.27400 #pixels= 716 in= 1



Selected Monomers



Selected >5mers

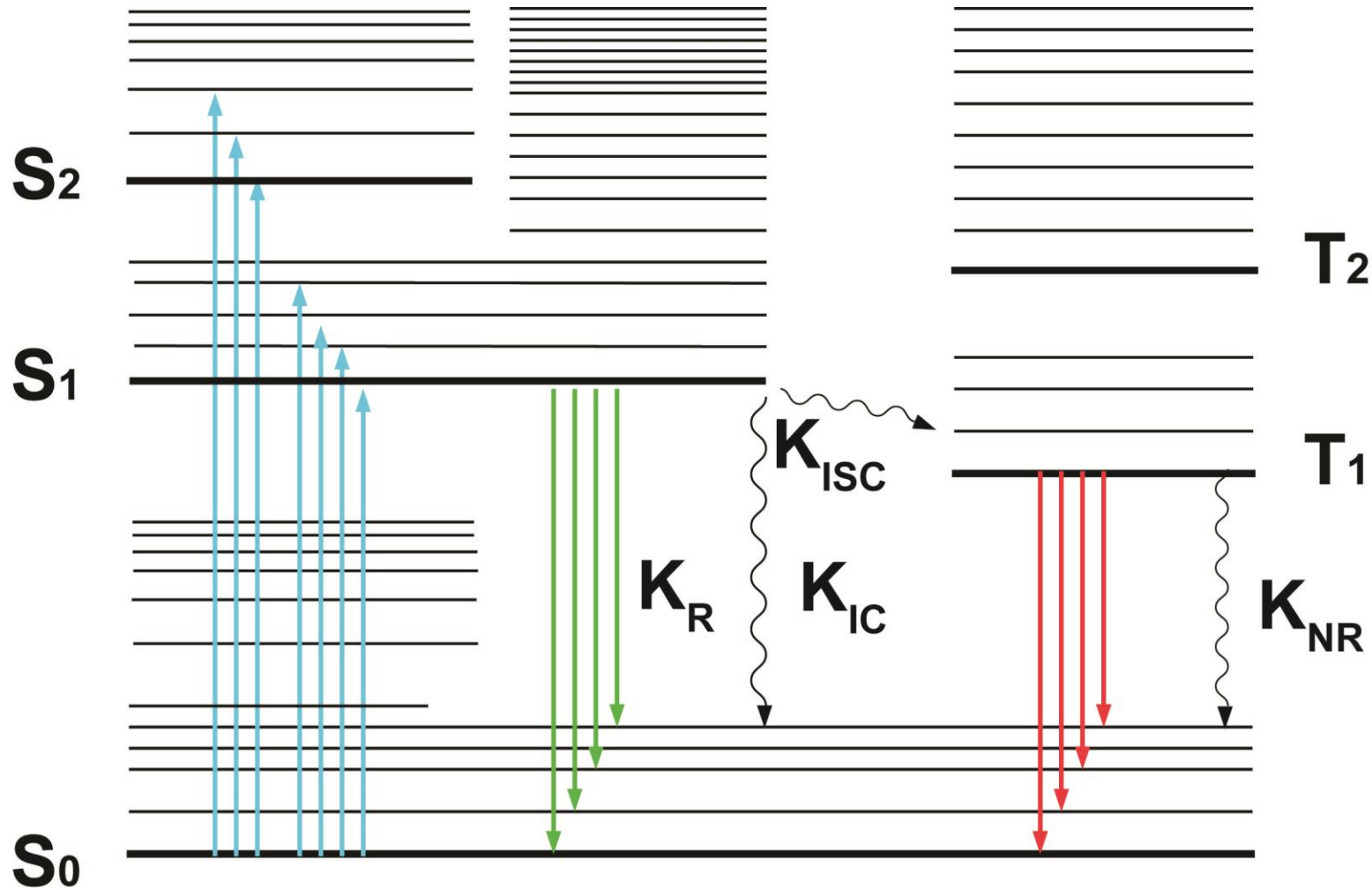


# Summary

- FCS provides the dynamics and the  $\langle N \rangle$  in the observation volume.
- PCH provides the brightness and the  $\langle N \rangle$  in the observation volume.
- N&B distinguishes between number of molecules and molecular brightness in the same pixel. The immobile fraction can be separated since it has a brightness value =1.



# Perrin-Jabłoński diagram





# What is the Lifetime?

Absorption and emission processes are concepts that involve a population of molecules. In general, if  $N_1$  is the population of the excited level  $S_1$ , the population is described by the relation:

$$\frac{dN_1}{dt} = -(k_R + k_{NR}) N_1 + f(t)$$

$$N_1 = N_1(0) e^{-t/\tau_S}$$

$$\tau_S = \frac{1}{k_R + k_{NR}}$$

$\tau_S$  is the lifetime of excited state  $S_1$

If a population of fluorophores is excited at time  $t=0$ , after a time the number of molecules in  $\tau$  is decreased to  $1/e$  or to about 36.8%

# Application to Förster Resonance Energy Transfer (FRET)

FRET strongly depends on the distance between the donor and acceptor:

Förster calculated the rate of transfer to be

$$k_T = \frac{1}{\tau_D} \left( \frac{R_0}{R} \right)^6$$

$\tau_D$  is the lifetime of the donor D in the absence of the acceptor A.

$R$  is the distance between the two groups

$R_0$  is called the Förster distance

$E$  is transfer efficiency (fraction of photons absorbed by the D and transferred to A)

$$E = 1 - \frac{\tau_D}{\tau_A}$$

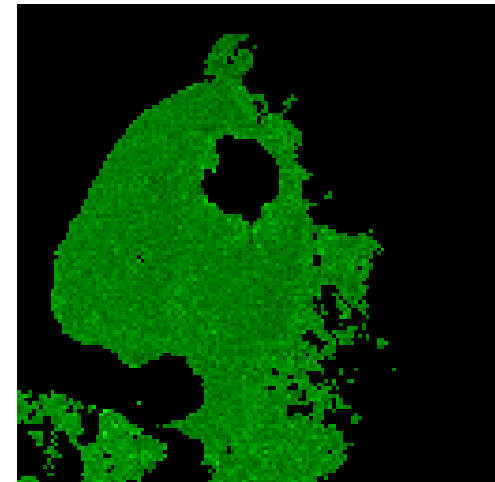
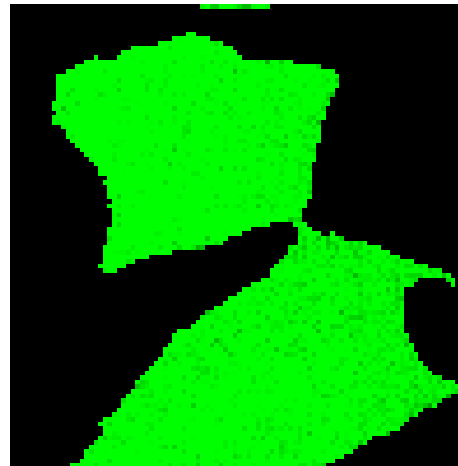
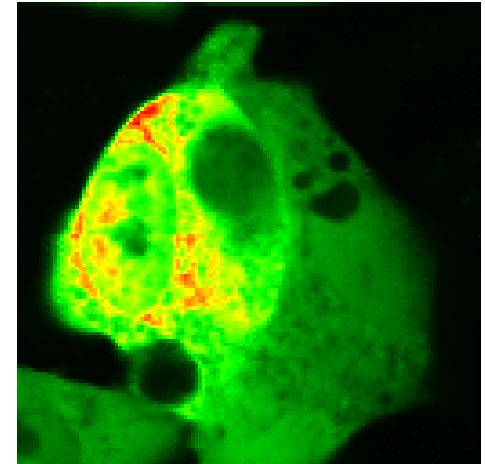
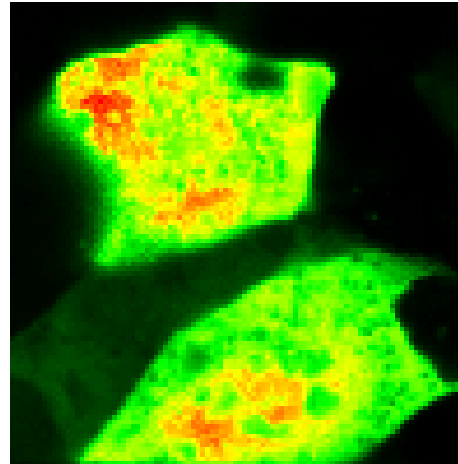
# FRET

Images of opossum kidney cells expressing a CFP (left column) and CFP/YFP tandem protein (right column).

Top: intensity

Bottom: phase lifetime

Left: 2.1 ns; Right: 1.5 ns

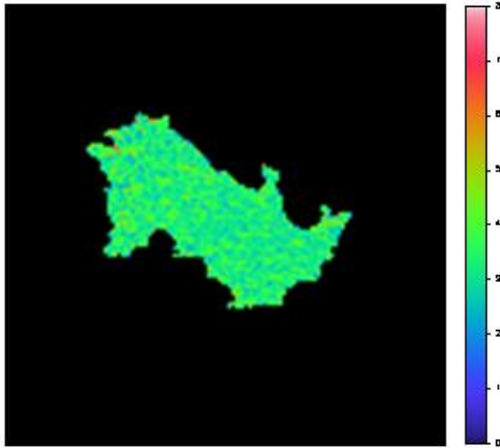


**Images** obtained in **frequency domain: Ti-Sapphire** – 2-photon exc. at 850 nm

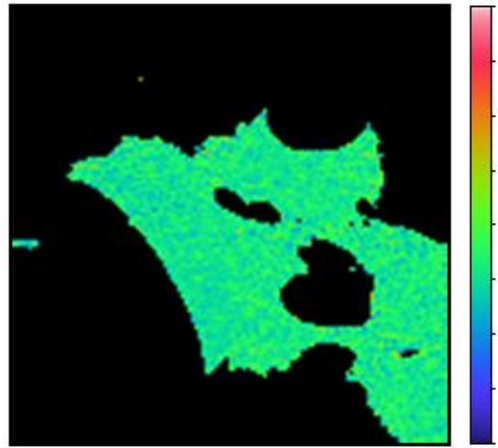
The images in channel 1 were collected through a 520 – 560 nm YFP filter and in channel 2 through a 460 – 500 nm CFP filter.

# Applications to Cerulean-Venus pairs FRET

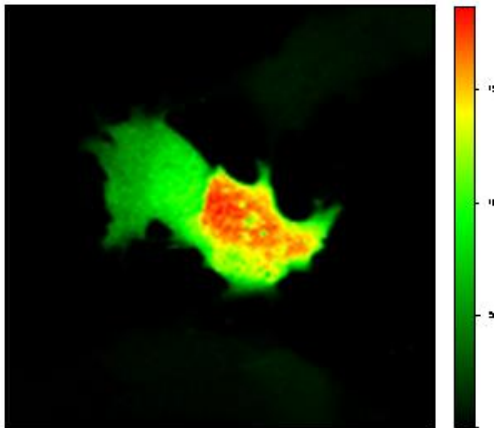
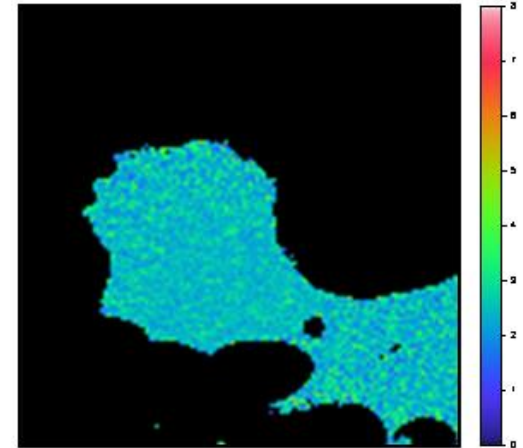
Cerulean



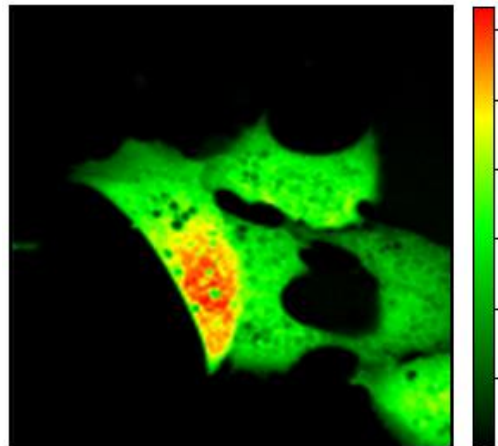
Cerulean 32-venus



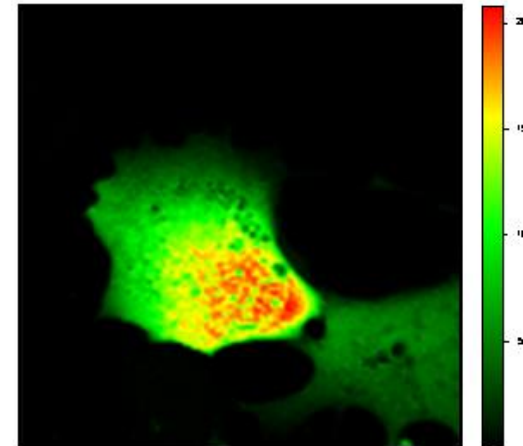
Cerulean 17-venus



$\tau = 3.06$  ns



$\tau = 2.63$  ns  
 $E = 14\%$



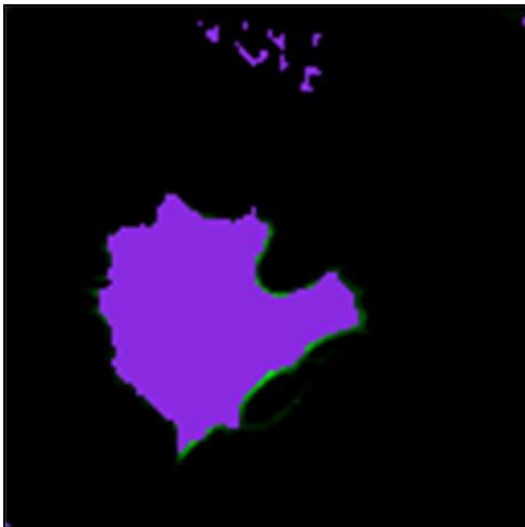
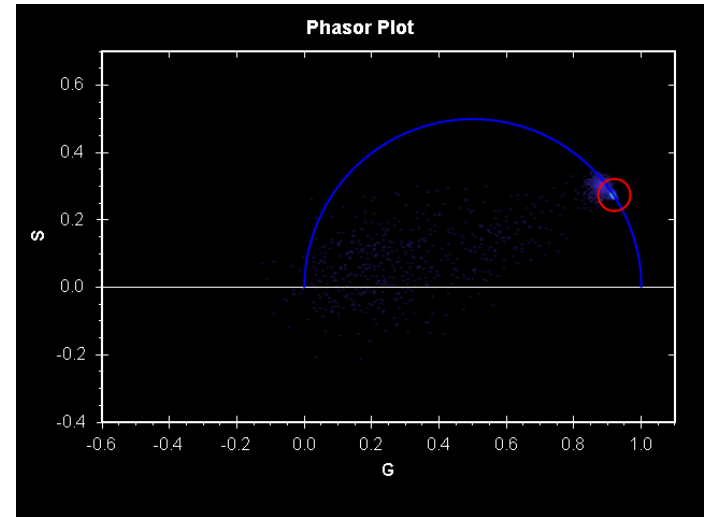
$\tau = 2.2$  ns  
 $E = 27\%$



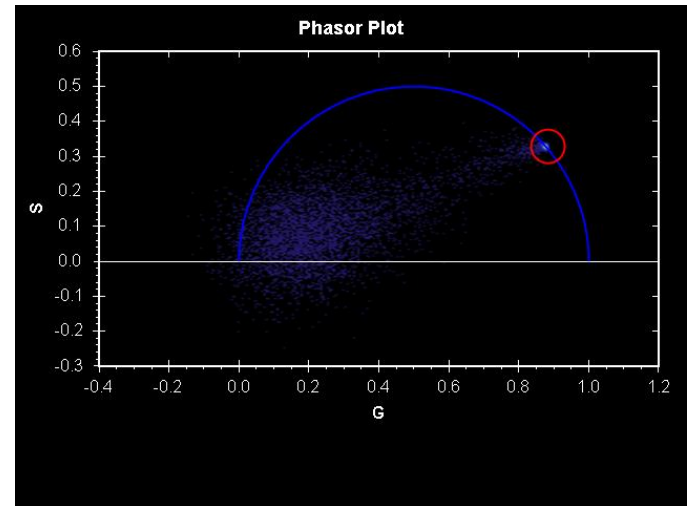
# Polar Plots



**C17v**  
**2.2 ns**



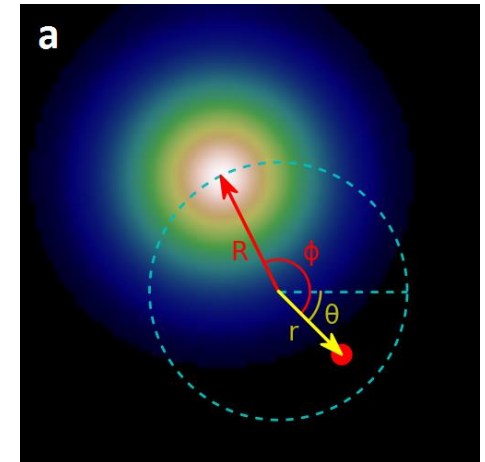
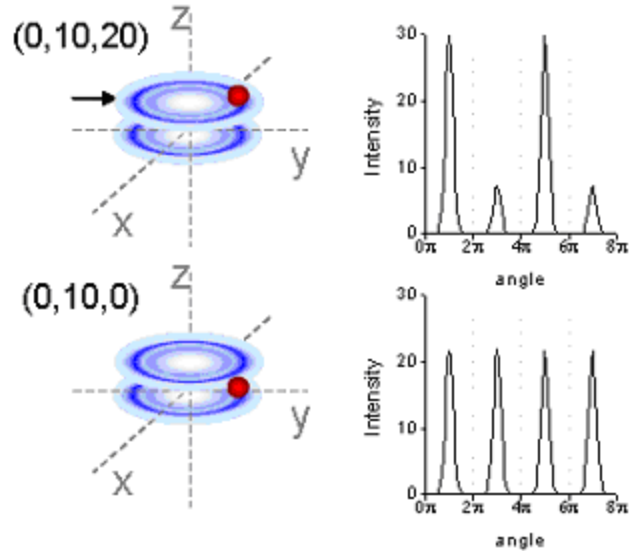
**C32v**  
**2.6 ns**



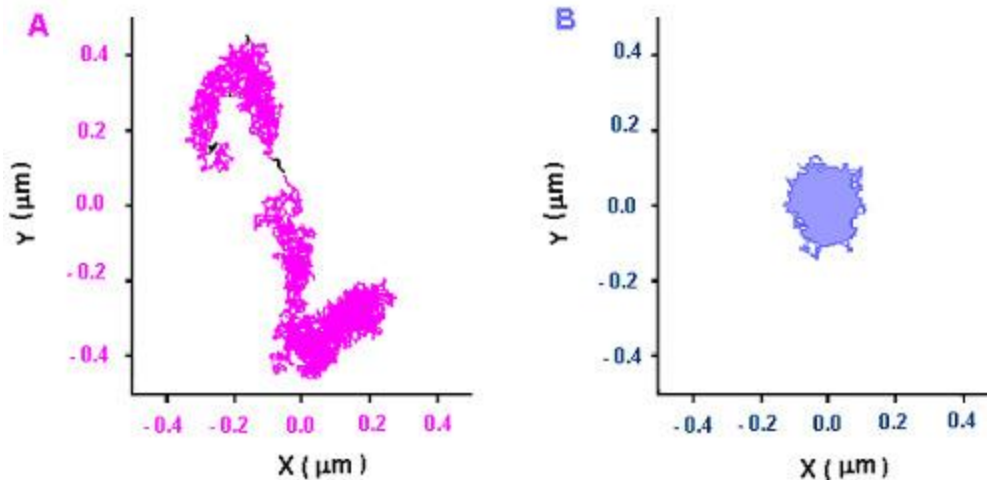
# Summary FLIM

- Lifetime measurements provide a powerful tool for the characterization of several processes in materials and life sciences
- The new DFD approach makes FLIM in cells faster and more sensitive
- The Polar Plot approach greatly simplifies the data analysis
- FLIM can be added to most commercial LSM

# Particle Tracking and Nanoimaging

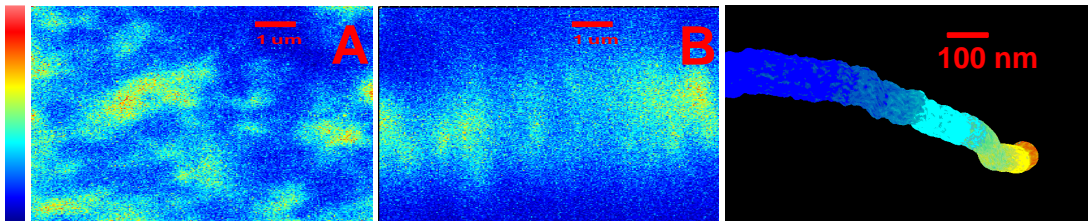
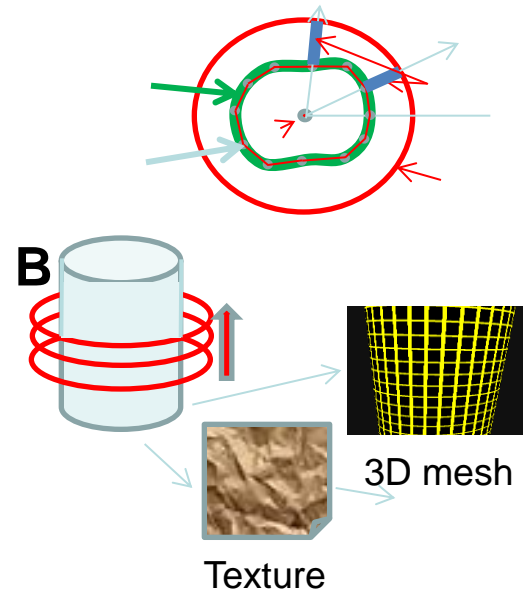
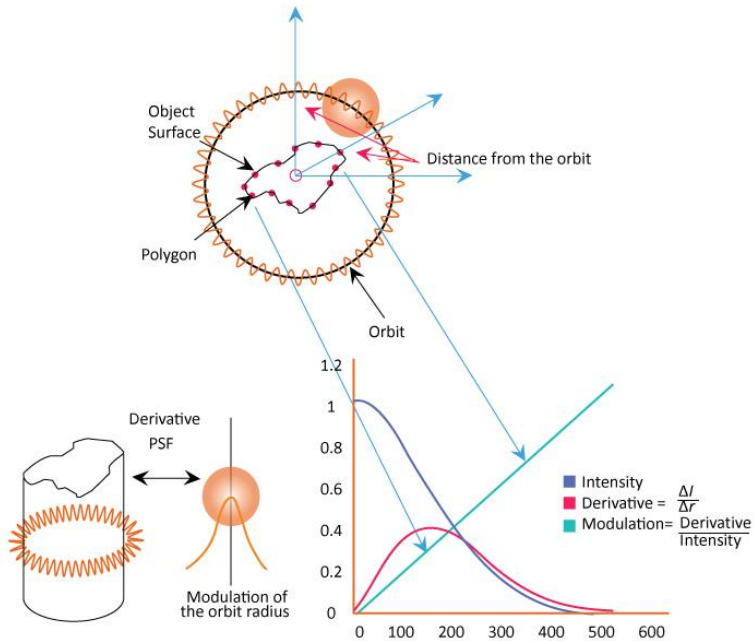


the radius of the orbit should be half of the width ( $\omega_0$ ) of PSF



Dynamics of chromatin in living C6-14 cells. Trajectories recovered in a control (A) and an azidetreated (B) cell.

# Particle Tracking and Nanoimaging





# What are the requirements on the instrumentation?

- Optics and microscopes
  - High-speed galvo-mirrors
- Light Sources
- Light detectors
  - Avalanche photodiodes
  - GaAs PMTs
  - Hybrid PMTs

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